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Enzymatic Electrosynthesis: An Overview on the Progress in Enzyme-Electrodes for the Production of Electricity, Fuels and Chemicals

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Abstract

Recent interest in the field of biocommodities production through bioelectrochemical systems has generated interest in the enzyme catalyzed redox reactions. Enzyme catalyzed electrodes are well established as sensors and power generators. However, a paradigm shift in recent science towards the production of useful chemicals has changed the face of biofuel cells, keeping the fuels or chemicals production in the upfront. This review article comprehensively presents the progress in the field of enzyme-electrodes for the production of electricity, fuels and chemicals with an aim to represent a practical outline for understanding the use of single or multiple redox enzymes as electrocatalysts for their electron transfer onto electrodes. It also provides the state-of-the-art information regarding the different existing processes to fabricate enzyme electrodes. Successfully-achieved electroeurzymatic anodic and cathodic reactions are further discussed, together with their potential applications. Finally, techno-economic and environmental elements for industrial processing with enzyme catalyzed bioelectrochemical system (e-BES) are anticipated, in order to provide useful strategies for further development of this technology.

Keywords: Electrodes; Immobilization; Electrosynthesis; Biofuels; Redox enzymes; Electron transfer

material. At the cathode, a reduction reaction of an electron acceptor which may or may not be enzymatically-mediated e.g. O, reduction can

Introduction

During the past decade, interest in bioelectrochemical systems (BESs) has significantly expanded. However, the major research focus is currently directed at microbial bioelectrochemical systems [1]. Enzymatic electrocatalysis involving energy applications has remained more discrete. However, the continuous search for highly selective, efficient and low cost non-precious catalysts, together with the recent advances in bioelectrochemistry and its related fields have already allowed further progress on enzymatic production of electricity from a wide variety of substrates or, the other way around, enzymatic applications of excess electrical energy for the production of chemicals and fuels [2].

Enzymes, contrary to microbes, have been the most important target for biosensor technologies. So, the electrochemical grounds for enzymatic applications are rather strong. Still, sensor operation is often desired at low current and potential differences, in order to avoid counter-reactions. On the other hand, energy applications demand maximum values of current and potential difference [3]. Furthermore, electricity-, fuel- or chemical-prospective devices are expected to have a stable and extended lifetime, which is still a crucial factor in the enzymatic-electrocatalysis-driven research of our days.

As an example of these technologies, Figure 1 presents a general scheme of current production in an enzymatic fuel cell. At the anode, enzymes can produce electricity and release protons from the oxidation of substrate fuels (e.g. glucose), while at the cathode substrate reduction (e.g. oxygen, carbon dioxide, volatile fatty acids) together with the use of electrons and protons can be completed for enzymatic electrolysis or electrosynthesis [4]. However, there are various critical fundamental challenges remaining unresolved in such processes. For example, the electron conduction between enzymes and electrodes still entails great improvement in the case of enzymatic bioelectrochemical systems (e-BES) [2].

At the anode, a reduced substrate (S_{red}) is oxidized (to S_{ox}) by means of an enzyme or enzyme-chain supported on an electrically-conducting



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be carried out over a Pt-based electrode or over a glucose-oxidase-based carbonaceous electrode, by using the electrons and protons released at the anode. Electricity is directly produced during this process. Otherwise, enzymatic conversion can be carried out at the cathode for electrolysis purposes when $E_{an}>E_{cat}$, for synthesis applications such as e.g. alcohol production from volatile fatty acid reduction. Paired electrolysis can also be achieved, producing other valuable compounds at both cathode and anode level. In some cases the anode and cathode compartments are separated by an ion-selective membrane, in others this component is not essential.

The major objectives of this review are (i) to present the progress of enzyme-electrodes for the production of electricity, fuels and chemicals, simultaneously understanding the use of single or multiple redox enzymes as electrocatalysts and their intrinsic electron-transfer mechanisms to electrodes; (ii) to provide state-of-the-art information regarding the different existing processes to fabricate enzyme electrodes (iii) to discuss successfully-achieved electroenzymatic anodic and cathodic reactions together with their potential applications. A special attention was focused on the possible enzymatic electrosynthesis mechanisms for the value-added product synthesis. Finally, technoeconomic and environmental elements for industrial processing with e-BES are projected, in order to provide useful strategies for further development of this technology.

The ABCs of enzyme-electrodes

Enzyme organization: Enzymes can be classified in several ways. The highest classification level is related to their function: a) oxidoreductases (redox enzymes) catalyze oxidation or reduction reactions, b) transferases transfer functional groups, c) hydrolases catalyze the hydrolysis of various bonds, d) lyases cleave various bonds by means other than hydrolysis and oxidation, e) isomerases catalyze isomerization changes within a single molecule and f) ligases join two molecules with covalent bonds [5]. In this article, focus will be only on oxidoreductases, since they are the sole enzymes capable of catalyzing the transfer of electrons from one molecule to another or to electrodes.

Redox enzyme systems: Oxidoreductases are a group of enzymes that usually utilize nicotinamide adenine dinucleotide (NAD) or its phosphorylated analog (NADP) as cofactors. However, they can also act on other groups of electron donors such as CH-OH, aldehyde or oxo, CH-CH, flavine adenine nucleotide (FAD) or its phosphorylated analog (FADP), CH-NH₂, CH-NH, etc. Similarly, it also can act on the other compounds such as sulfur, heme, diphenols, peroxide, hydrogen as well as single or paired donors with incorporation of molecular oxygen, superoxide radicals, CH or CH₂, iron-sulfur proteins, reduced flavodoxin, phosphorus or arsenic and all the X-H and Y-H to form an X-Y bond among others. So far, the most relevant enzymes in e-BES have been oxidases, (de)hydrogenases and peroxidases. Redox enzymes typically contain one or more coenzyme structures that act as catalytic active centers. Flavins and Pyrroloquinoline Quinone (PQQ) are most commonly known coenzymes. All these enzymes typically undergo Mediated Electron Transfer (MET) or Direct Electron Transfer (DET). In addition to organic species, metalloproteins containing metal coenzymes are also used, e.g. copper, nickel-iron-sulfur, iron-sulfur, and heme-based. Cytochromes are commonly studied co-factors in BES and they are electron transport proteins containing heme groups [3].

Enzyme function in e-BES: Based on the function of enzymes, e-BES can be classified into two broad categories, direct energy producing and value-added product synthesizing. The enzymes that participate in the

electron transfer chain between the fuel and the anode from oxidizing the organic matter with their simultaneous reduction at cathode in presence of an oxidant. This is the same principle as conventional or Microbial Fuel Cells (MFCs). On the contrary, the product synthesizing e-BES consists of enzymes that are involved in electroenzymatic synthesis of chemicals and fuels with the help of energy generated [6]. Although electricity generation in e-BES is rather interesting, up to date no commercial alternatives are available at the industrial scale. However, the use of enzymes in organic synthesis has shown great potential. So far, more than 150 industrial processes are known, where enzymes are used for the production of fine and commodity chemicals [4]. It is anticipated that enzymatic electrosynthesis will also rapidly expand to fulfill industrial needs in green chemistry.

Mono-enzyme vs. multi-enzyme electrodes: Compared to e-BES, the microbial Bioelectrochemical Systems (m-BES), using bacteria as electrocatalyst, already contain a wide variety of enzymes that allow complex oxidation or reduction processes for a great variety of substrates. On the contrary, most e-BES employs a single enzyme to partially convert a specific compound [7]. In general, a single enzyme can catalyze a simple chemical reaction, and approximately 4800 enzyme entries have been documented and classified to date [8]. Most single redox enzymes catalyze one- or two-electron reactions, and represent a single elementary step in more complex reaction mechanisms; although some enzymes (e.g. blue copper oxidases: laccase, ascorbate oxidase) catalyze four-electron reduction of oxygen to water, higher specificity is usually desired [3]. Relatively complicated chemical reactions can be mediated by multiple enzymes in one location (Figure 2). The use of multiple enzymes in one location has numerous benefits such as fewer unit operations, smaller reactor volume, high volumetric and spacetime yields, shorter cycle times and less waste generation. Besides, with multiple enzymes working together, the equilibria among the reactions is usually regarded as unfavorable which can be driven to the formation of target products [8]. Multi-enzyme-bioelectrochemical systems (me-BES) can be considered a type of in vitro synthetic biology project, promising for the production of fuels, chemicals, biocommodities and bioelectricity [8].

Electron transfer mechanisms

Electrons generated during oxidation should reach the anodic electrode to enter into the power circuit. Similar to the m-BES known as MFCs, there are two different mechanisms that have been proposed for anodic electron transfer in e-BES (Figure 3), as earlier introduced, DET and MET (section 3.1.2) [9-11]. However, the enzymatic electron transfer processes have their singularities. In general, the enzymes will have two distinct sites, *viz.*, the biocatalytic site (apoenzyme/protein



Figure 2: The functional difference between the mechanism of mono vs multiple enzyme electrodes [S: Substrate; P: Product; E: Enzyme; I: Intermediate; e-: Electron].





Figure 3: Schematic illustrating a simple arrangement for (A) direct electron transfer (DET) and (B) mediated electron transfer (MET), between the active site of an electrochemically-active enzyme and a solid electrode, during the oxidation of a substrate (Re-printed after [30] with permission from Elsevier).

part) for substrate recognition and the electrocatalytic site (prosthetic group/redox mediator) for electron transfer. The prosthetic group or internal redox site of the enzyme undergoes a conformational change during electron transfer, described as DET. However, some of the enzymes have only one site for both activities, which generally uses an external soluble redox carrier for electron transfer, described as MET. Overall, electrons derived from the enzymatically catalyzed oxidation of a substrate by oxidoreductases are transferred to the electrode through reduction of either a prosthetic group integrated within the enzyme (DET) or a co-substrate (MET), intermediately storing the transferred redox equivalents. However, the possibility to re-oxidize the prosthetic group or the co-substrate is crucial in order to regenerate the enzyme activity and make it available for further substrate recognition and conversion reactions [12]. Moreover, it is very difficult to clearly delineate the differences between MET and DET [12]. The detailed mechanism and existing challenges are discussed in the further sections.

Direct electron transfer (DET): The simplest and most appealing mode of interaction between electrodes and enzymes is DET, due to small number of transfer steps. In this form of electron transfer, the redox enzymes that possess tightly bound cofactors in the active site, can deliver the electrons directly at the electrode. The first reports on DET were published over 30 years ago [13] and recent reports are also available on a wide range of enzymes [14-18]. DET has been reported for about 40 redox enzymes, including laccase, peroxidases and complex multi-cofactor-containing enzymes [13]. Most extensively studied and best characterized enzymes for DET belong to the group of peroxidases [19-29]. Though there exist several mechanisms for the direct electrochemical communication between enzyme and electrode, several challenges need to be overcome to achieve significant rates of electron transfer, leading to appreciable current densities, between active sites and solid electrode surfaces. Major criteria for the effective electron transfer are shorter ET distance between enzyme and electrode and right orientation of the enzyme active site towards electrode.

The electrode surface itself is considered to be a "substrate" for the enzyme during DET, where the electron transfer kinetics are controlled by—at least—the electrode potential and by the distance between the surface and electron transfer structures in the enzyme [30]. DET involves the direct electrochemical recycling of the prosthetic group of the enzyme at the electrode surface, sometimes involving an electron

tunneling mechanism. The mechanism of tunneling is based on a "bridge" molecule of complex structure (including different functional groups), that simply represents a barrier for ET which tunnels deep under the barrier. Superexchange is also a DET process similar to tunneling, but in a system with vacant electronic energy levels, higher than the energy of the tunneling electron. However, for this case, the electron transfer between two redox enzymes is not only dependent on the difference in potential between them and the distance between their respective redox centers, but also on the structural rigidity of the redox species involved [31,32]. The electron transfer distance between the prosthetic group of the enzyme and the electrode surface is obviously long due to the shielding provided by the protein shell, and this makes DET via tunneling a bit difficult. Although, immobilization of the redox enzyme on the electrode reduces the ET distance, negligible rates of ET have been observed for distances beyond 2 nm, which are very difficult to achieve. This indicates that DET can only take place when an electrode is placed within this distance to an enzyme cofactor in the active site [33]. Upon immobilization, the electrode can also block the access to the active site of the co-substrate/substrate resulting in no bioelectrocatalytic current for substrate electrolysis, even when an electrode can approach sufficiently close to an active site to achieve DET. Moreover, the denaturation of enzyme structure during immobilization with the consequential loss in activity, is another hurdle [12,13,34], caused by weak and unstable binding, random surface orientation, or impeded by the multiple redox sites present in a single enzyme [13,34]. Thus, an optimally designed electrode configuration has to ensure that the ET distance between an immobilized redox protein and a suitable electrode surface is made as short as possible but with favorable orientation. The enzyme molecules immobilized in the first monolayer on an electrode surface tend to show higher DET, but only a very small number of enzymes can be productively immobilized on the electrode surface which limits the overall electron transfer. In addition, proteins directly adsorbed on carbon, platinum or gold surfaces tend to denature, leading to electrode fouling and to unfavorable conditions for electron transfer [12].

Similarly, for enzymes that have their active sites sufficiently exposed to permit DET, the correct orientation of each enzyme at the electrode surface is a pre-requisite to keep the closest distance between enzyme and electrode. Design of suitable surfaces for the anisotropic and oriented immobilization of enzymes, such as immobilization on self-assembled monolayers (SAMs), is one approach to enhance

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DET. Orientation of immobilized enzymes with the prosthetic group directed towards the electrode surface also drastically increases the rate of DET. The immobilization of an enzyme on a SAM also leads to the orientation of its prosthetic group towards the electrode surface and thus to a shortened electron transfer distance [12,35,36]. In addition, the SAMs also help in preventing denaturation of the proteins at the electrode surface [12].

Another approach for enhanced DET is the entrapment of enzymes in the conducting materials. These conducting matrices can also increase the "virtual" electrode surface by allowing the enzymes to immobilize at a fair distance from the electrode surface to take part in effective DET [12]. Entrapment into conducting materials such as solgel composites, polymers, etc., has been described previously [37-42]. However, the sensitivity of the enzyme has shown to become low in some cases after entrapment, and the ET mechanism could not be well defined as DET [43-45], except in very few cases [46].

Apart from these proposed mechanisms, another alternative for DET includes ET in a multi-cofactor enzyme with multiple subunits. This DET route is based on the pathway between the active site of the enzyme and the electrode surface, consisting of several steps between the different cofactors within the subunits of the enzyme. The studies related to multi-cofactor enzymes (mainly PQQ, FAD and heme-containing) reveal the priority of the distance separating the active site from the electrode [47-55]. However, proper immobilization of these enzymes on the electrode surface without losing any of the properties is

a tough task. SAM-modified surfaces can also be used as a basis for the design of new ET cascades, as the distance between the active site and the electrode surface can be tailored. However, design of "molecular cables" by the integration of redox relays into the monolayer or by introducing the conducting oligomers with in the spacer chain to subdivide the overall ET distance, will result in enhanced electron recovery at the electrode surface through DET [12,56].

Mediated electron transfer (MET): Mediated electron transfer (MET) is an alternative to the DET, where a co-substrate or an electrochemically active chemical species (e.g. redox mediator) can be used to shuttle the electrons between the enzyme and the electrode. Mediators are artificial electron transferring agents that can readily participate in redox reactions with biological components. They form low molecular weight redox couples, which shuttle electrons from the active center of the enzyme to the electrode surface or vice versa [57]. Mediators are quite diverse in structure, properties and redox potentials (Figure 4). Their electron transfer, therefore, can be generally classified as homogeneous- and heterogeneously-mediated transfer. Homogeneous mediation occurs in solution, where both the mediator and the enzyme diffuse freely in the medium and after the electron transfer both the enzyme and mediator remains in the solution phase and then the free mediator interacts with the electrode. On the contrary, heterogeneous mediation implies diffusion of the mediator or the enzyme through an interface, keeping the other on the electrode, before and after achieving electron transfer between them.



Figure 4: Cofactor structures and redox processes for: (A) FAD/FADH₂, (B) NAD⁺/NADH and (C) PQQ, where R links adenosine diphosphate via ribitol to the flavin (A) or nicotinamide (B). (Re-printed after [30] with permission from Elsevier).

The latter occurs when the mediator is added to the bulk solution for reaching an immobilized enzyme or when the mediator is present on the electrode and not in the bulk solution, that contains the enzyme [3,57]. Initial studies on MET focused on the solution-phase mediators, which necessitate inclusion of a separating membrane between anode and cathode to prevent short-circuiting and cross reactions. Therefore, immobilization of mediator and enzyme onto electrode is preferable for the miniaturization of devices, permitting exclusion of the membrane. Initially, the freely diffusing natural co-substrate (NAD⁺) was used as electron shuttle between the enzyme and the electrode (to recycle the prosthetic group of enzymes), based on the fact that these co-substrates can be reduced or oxidized at a metal-electrode interface [12]. However, the regeneration of the co-substrate is energy intensive (which decreases the cell potential) and also condition dependent. Introduction of artificial redox mediators was found as an alternative to this mechanism, as they lower the working potential resulting in decreased interference by other compounds that are directly oxidized/ reduced at the electrode surface [12,58,59].

Ideal mediators should react rapidly with enzymes and exhibit reversible heterogeneous kinetics. Also, the overpotential for mediator regeneration should be low and pH independent. The mediator should have stable oxidized and reduced forms; the reduced form should not react with oxygen, while the oxidized form should not react with protons, if such are not the targeted reactions [57]. If these conditions are met, different mediators and prosthetic groups can be used for substituting or reducing expensive natural mediators of particular enzymes, allowing more economically efficient processes, if not also more kinetically favorable [60]. The artificial redox mediators are generally low molecular weight, soluble metal complexes with reversible electron transfer properties such as $K_{4}[Fe(CN)_{c}]$, quinones, Os-complexes, etc. [61-67]. These artificial mediators also help in the regeneration of co-substrates which cannot regenerate on the bare electrode surface (NADH), especially at lower potentials [12]. Further to this approach, the adsorption of soluble redox mediators on the electrode surface followed by the immobilization of the enzyme in a second layer has been carried out [59,68,69]. However, this mechanism is similar to the freely-diffusing soluble mediators mechanism as these mediators diffuse between enzyme and electrode. Moreover, leaching of the mediators, lack of long-term stability, and sample contamination, are the main disadvantages in this mechanism [12,70,71].

The free diffusional movement of the redox mediator is obvious and an indispensable prerequisite for a productive electron transfer. Henceforth, it is important to maintain a fast electrochemical communication between enzyme and electrode as well as to tightly retain the redox mediator at the electrode surface. One approach to satisfy these two conditions is known as "hopping", where electron transfer distances are reduced by dividing the overall ET process into a sequence of electron hopping reactions between redox mediators (relays) covalently attached to a matrix. The ET mechanism in hopping is dominated by a sequence of self-exchange reactions between adjacent redox mediator molecules. However, care should be taken so that the rate of these self-exchange reactions should not limit the electron transfer [12,13,72]. Similarly, covalent binding of the redox mediator via long and flexible spacer chains either to the electrode surface (seaweed mechanism) or to the outer surface of the enzyme itself (whip mechanism), has also been proposed as alternative [12,73]. Mixing the mediator into the carbon paste (graphite powder) is a relatively easy and effective method of mediator integration [74-81]. These carbon pastes can be further modified with stabilizers [82] or polyelectrolytes [75] to increase the long-term stability, response time, etc. The enzyme can also be mixed into the paste, but it is mostly immobilized on top of the carbon paste surface to increase the contact with the substrate. There are other approaches proposed to retain the redox mediator or enzyme at the electrode and prevent their leakage, such as trapping them within ion-exchange membranes [83-85], manufacturing them as colloidal particles [86], physical entrapment of the redox mediator into the matrix of composite electrodes [87,88], and entrapment into hydrogels [89] or in conducting polymers [90,91]. However, all these strategies have not completely solved the problem of mediator leakage and, in consequence; it has become indispensable to bind the mediators covalently in order to establish an electron-hopping mechanism instead of a shuttle mechanism [12]. Development of electroenzymes is another recent approach, where the protein itself is modified with covalently bound redox mediators at the outer surface [92-95] or at the inner surface of the protein, preferentially in close proximity to the active redox cofactor of the enzyme [96-99]. The covalently bound redox relays are supposed to shorten the ET distance between the deeply buried active site and the protein surface by allowing hopping mechanism via the enzyme-bound artificial mediators.

Irrespective of the mechanism, thermodynamic redox potentials of mediator(s) will dictate the power output during MET in fuel cell mode. More positive oxidative biocatalysis at anode and a more negative reductive biocatalysis at cathode drive the electron transfer between enzyme active site and mediator but will contribute to the loss in cell voltage. Therefore, achieving a best compromise between driving force and current generation is a major challenge in MET, in order to maximize the power output [12,13,100]. This can also be extrapolated as more energy consumption in electrolytic e-BES, which is quite relevant since more than 80% of the operational costs of electrolysis systems typically account for energy consumption. The electron transfer kinetics between the enzyme and the redox mediator should also be as fast as possible (i.e. high exchange current density) to compete with the regeneration of the enzymatic active site.

The absence of mediators is a big advantage when it comes to selectivity (there is less susceptibility to interferences due to lower electrode potentials) and because of the elimination of one reagent in the reaction sequence [13,57]. However, addition of a mediator may potentially increase the maximum rate of electron transfer, compared to DET. The mediators serve to facilitate a biological electron transfer, which is favorable thermodynamically but not kinetically [68]. Additionally, by using mediators the enzyme does not need to be in direct contact with the electrode surface, which minimizes enzyme denaturation possibilities. High electron transfer rate constant (k_{ET}) with the enzyme and accessibility in terms of steric effects, orientation and distance dependence, are two major factors to be considered while selecting mediators in order to obtain high currents [57,100]. Redox potential, electrostatic interactions, pH and ionic strength are also the other factors that play a major role on facilitating MET.

Development of enzyme immobilized electrodes

Enzymes are usually sensitive and their lifetime is limited but their stability over a long period of time is much crucial for their applications [101,102]. Immobilization of the enzymes onto the solid conductive matrices is an efficient and sustainable solution to confer a high stability and extended lifetime. It protects the enzyme from various external environmental conditions, such as shear forces, pH, temperature fluctuations, organic solvents, toxins, etc., [103]. Furthermore, immobilization affords a high concentration of enzyme moiety on the electrode, as well as easy handling of the e-BES along with the possibility of increased re-use of enzyme [104,105].

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Henceforth, it can be concluded that immobilization of an enzyme offers a valuable solution for e-BES design and operation. In fact, the proper implementation of enzyme-electrodes relies mostly on the immobilization of enzymes or electrochemically active chemical species (e.g. mediators) and the chemical and physical properties derived thereof [6]. Immobilization of the enzyme on the electrode must be sufficiently strong to facilitate the transfer, but still suitable for not causing denaturation. Also, the enzyme must be properly oriented with respect to the electrode surface such that the active center is overlapped within an acceptable distance for the electron transfer to occur [3,72]. The electrode surface must be designed to resemble the surface characteristics of original environment (e.g. surface charge distribution or hydrophilic/hydrophobic properties) which facilitates the efficient interaction between enzyme and electrode without dramatic conformational changes [13].

Bare enzyme immobilization over electrodes has been the most common approach studied to achieve higher electron transfer. However, there are several other strategies, such as immobilization on the electrodes modified with promoters, SAMs of alkanethiols, polyelectrolytes, surfactants and ionic liquids, have also been used [13]. Enzymes with given surface groups suitable for direct chemisorption such as the thiolate and the disulfide group offer an attractive approach to protein-immobilization in well-defined orientations. The covalent, electrostatic or hydrophobic linking group may be close to the electrochemical redox center and this would support facile electrochemical electron transfer [72]. Despite the large record existing on enzyme-based electrochemistry (especially in the context of biosensors), the fabrication of bio-catalytically-modified electrodes with enzymes is still in early stages, particularly because of the difficulties in reaching high enzyme stability and power output. In recent years, studies on the development of new materials, enzyme modification, understanding the mechanisms of enzyme catalysis, enzyme immobilization methods, enzyme electrode structures and ways of preparation, have been carried out with the purpose of improving the performance of enzyme electrodes [6].

Numerous studies have been performed towards the development of enzyme-immobilized electrodes and their applications. The enzymes should be immobilized in such a way that electronic states in the surface material and enzyme active center overlap, increasing the probability of electron transfer across the interface [3]. Furthermore, care should be taken during immobilization in aspects such as enzyme orientation with the electrode, stability and activity after immobilization, possible denaturation during immobilization, etc. The methods of immobilization (Figure 5) developed over years can be broadly classified into three major groups, i.e. adsorption, covalent binding and entrapment [106-108]. Some of the previous studies reported about these methods in detail [2,109,110]. These immobilization methods are commonly used to construct bioactive hybrid materials and devices, including bioelectrodes for biofuel cell applications. However, there are certain challenges still needs to be addressed in the methods of immobilization. This part of the review mainly focuses on these existing challenges and various materials used for immobilization in a broader context.

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Challenges in Immobilization: Though, there is enormous literature available on the immobilization technology, still there are certain constrains to be overcome to make it industrially applicable. The major challenges can be summarized as, maintenance of enzyme activity, stability over changes in physico-chemical factors, enzyme life-time, right orientation of enzyme active center on the electrode surface, synergistic interaction of the enzyme with the electrode after immobilization, among others [103]. A recent review on immobilization technology by Yang and co-workers has thrown some light on the existing methods and the materials for enzyme immobilization including the challenges and the future scope [111]. Adsorption is very easily adapted and well-studied method but has the enzyme leaching problem. Similarly, covalent binding is known for enzyme stability but has a problem of lower activity after immobilization. Arrangement of enzymes in different layers and synthesis of enzyme-electrodes are the two major approaches that can be pursued for the better immobilized moieties. Immobilization structures strongly influence mass transfer in the e-BES in terms of substrate diffusion through the active sites, the electron transfer and diffusion of redox mediators [111]. High resistance for the mass transfer process in biofuel cell necessitated the development of designed immobilization structures which may help to alleviate the mass transfer problem. The increasing interest in nano materials and the involvement of multiple disciplines towards biofuel cell development has put forward the progress in using various nanostructures, viz., nanoparticles, nanofibers, nanowires, nanotubes, nanosheets, nanopores and nanocomposites, because of their larger surface areas, short charge diffusion lengths, and fast diffusion rates, etc. In general, the large surface area of nano structures leads to possibility of high enzyme loading and thus resulting in improved power density. Furthermore, these nanostructures also help in extending the lifetime of the biofuel cells by increasing the enzyme stability and activity under higher mass transfer rates. However, these nano-materials can be arranged into different layers for further enhancement in the process.

The direct usage of nanoparticles, which have high electronic and catalytic properties for the enzyme immobilization for effective synergetic functions. For example, Au nanoparticles have been used to prepare biocatalytic electrodes for biosensor applications via a codeposition approach with redox enzymes/proteins on electrode supports [112-123]. One-dimensional nanostructures such as fibers and tubes



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have been also studied recently for their potential in nanoelectronic devices. For example, electrospun nanofibers provide a large surface area for the attachment or entrapment of enzymes and reduce the substrate diffusional path leading to better enzyme activity [124-136]. These electrospun carbon nanofibers were also studied in MFC, for their efficiency, and showed higher electroactive microbial biofilm growth [137]. Similarly, carbon nanotubes (CNTs) also made a great impact in the field of e-BES for stable and active enzyme immobilization systems with its high specific surface area which helped in effective adsorption of the enzyme molecules [138,139]. Multilayered enzyme assemblies on solid conductive supports (electrode) are another approach using nanolayers and sheets. Initially, enzyme layers were made in contact with nanolayered immobilization-support materials under controlled enzyme deposition, through electrostatic interactions or through crosslinking (affinity interactions) or through encapsulation in matrices (tailored organized biomaterial layers) [111,140-147]. For example, reconstitution of the apo-enzyme on the electrode surface with surfacebound and electrochemically active prosthetic groups was shown to be an effective way to achieve higher electron transfer rates by glucose dehydrogenase on PQQ-modified surfaces [13,141,142]. Apart from these, nanoporous materials with high specific surface areas, multiscale porosity, tunable pore sizes, interconnectivity and rich surface chemistry were also have been studied for enzyme immobilization [111,148,149]. For example, enzymes immobilized on mesoporous materials and their applications in e-BES [2,150-152].

Even if layered structures for e-BES have shown efficient electron transfer, they are also not ideal because the amount of immobilized enzyme is small, due to monolayer covalent binding. Moreover, the thicker or higher the number of monolayers, the more elevated electric resistance develops on the interface, which adds to the ohmic drop within the system. Similarly, the catalytic activity will depend on the orientation of the enzymes and distribution of mediator molecules, if the latter are used in the system [6]. Conducting redox polymers can be a solution to overcome these limitations. Polypyrrole and polyaniline (emeraldine-base) are commonly applied in BESs [153]. They have unique properties for facilitating electron transfer, even over insulating basal nature of the materials, and were proven to enhance the current densities in both e-BES and m-BES systems [6,153]. They also showed an improved selectivity and stability over the others. However, the use of polymer-mediators has raised concerns on biocompatibility for implantable-device applications [6]. Besides, these immobilization methods essentially involve the use of chemicals, which add costs to the fabrication process. Similarly, the synthesis of electrodes (entrapment) is generally considered a rather expensive process and not easily scalable. Therefore, it is important to put some effort on the elaboration of new and more efficient means for their production. Moreover, enzyme electrodes become even more difficult, since they generally involve (as described before) the use of a variety of chemicals, high temperatures, among other difficulties. From this perspective, low-temperature calendaring (cold rolling) appears as an interesting alternative because it is simple, low cost, well known in the industry and easily scalable [154,155]. Surprisingly, its application on the fabrication on enzymeelectrodes is minimally used although ongoing research on the group of the authors of the present manuscript aims to confirm this direction.

Immobilization materials: The materials used for immobilization in e-BES are also considered to be critical and they must be capable of extracting or bringing the electrons from or towards the active site of enzyme, respectively. The bioelectrocatalytic efficiency of an immobilization material is largely governed by the electrical conductivity and hence it is the primary concern for the selection of an immobilization material along with the hardness of the material. In general, solid supports such as gold and platinum are considered as immobilization materials but with advancement in materials sciences, the application of polymers, carbons, oxide and metallic nanomaterials, sol-gel based materials and composite materials are also being used as efficient immobilization materials in e-BES.

Polymers

A variety of polymeric materials, *viz.*, Nafion, chitosan, polypyrrole, polyaniline, polyphenol, polythiophene, poly-1,3-phenylenediamine, polyvinyl pyridine, polyvinyl alcohol, polycarbonate, and nylon, have been studied as immobilization materials in e-BES [156-161]. Conducting electro-active biocompatible polymers are widely used as immobilization materials because of the guaranteed electron transfer which sustains the electrocatalytic reaction of the enzyme [162]. Similarly, use of efficient mediators such as osmium containing redox polymers has also been studied for effective electron mediation at anodes as well as cathodes [163-168]. Although there are limitations for this kind of approach in human applications due to the toxic effects of the metals, perhaps there is room for application of these materials at industrial level for the enzymatic electrocatalysis for the synthesis of commodity and fine chemicals.

Similarly, some functionalized polymers have been studied for immobilization of electrochemically-active enzymes. Nagel et al. studied electro-deposition of the polymer over a support which was functionalized by amino groups, followed by subsequent coupling of the biomolecules via the carboxylic group of the protein cross-linked by carbodiimide. They studied their function as enzyme immobilization matrix as well as binder and electron transporting mediator [169]. Electrospun nanofibers are also proved as promising material for the encapsulation of nanoparticles, enzymes, proteins and whole cells. Cells and enzymes encapsulated within electrospun nanofibers can be a straightforward and cost-effective method as well as they can play a role on controlling the viscosity of the electrolyte solution [170-173]. Polymer-brush-modified electrodes were also studied for their application in e-BES but the activity is dependent on the pH of the solution [174]. The polymeric materials are also employed to achieve additional functionalities such as receptors in the form of a polymer matrix, mediators, or as ion-selective membranes [175].

Carbon based materials

Carbon based materials are attractive electrode supports because of their unique properties such as large surface area, high electrical conductivity, high electron delocalization, and high chemical and thermal stability [111,176]. Immobilization of enzymes has been studied on a wide variety of high-surface area carbon materials, including carbon blacks, carbon pastes, nanotubes, nanofibers, graphite, carbon fibers, clothes and paper, glassy carbon, carbon aerogel, mesoporous carbon and reticulated vitreous carbons. Carbon nanofibres showed as good electrode supports in e-BES for effective enzyme immobilization and their conductivity facilitates diffusion of free electrons [177,178]. CNTs with high electrical conductivity have been also studied as electrode materials and showed to help in mediating electron transfer reactions. CNTs can also be introduced as efficient molecular-scale "conductive wires" between the electrode surface and redox enzymes, such as GOx and NiFe-hydrogenase to increase electron transfer [72]. Alternatively, a free suspension of support materials with enzyme (and mediator, if necessary) can be deposited on a porous support. This procedure allows profound mixing of enzyme with carbon nanotubes prior to deposition, but it is limited regarding the types of structures

that can be achieved after introduction of the enzyme. Majorly, two applications in the utilization of CNTs are commonly studied i.e. CNTs with metals (Pt/Au) and CNTs with polymers [179-182]. Carbon aerogel possesses high porosity, a large surface area and is extensively utilized as an enzyme adsorbent and electron conducting material [183]. For example, a laccase-adsorbed carbon aerogel electrode remained very stable without loss of the enzyme activity. Nanoporous structures of carbon aerogel have the advantage of stabilizing the enzyme electrode and they hold great interest in wastewater treatment [184,185]. On the other hand, graphene has several advantages for its application in e-BES, viz., superior electrical and heat conductivity, mechanical strength and unique optical absorption, and can thus be used as a novel class of electrode material [186,187]. However, graphene is hydrophobic and easily forms agglomerates irreversibly which is the limiting factor for its exploration as graphene-modified electrode. Similarly, mesoporous carbon with controlled porosity, high pore volume and large surface area, was also given much attention for e-BES applications [188,189]. Mesoporous carbon materials can be used in biofuel cell by enzyme cross-linking or by highly ordered mesoporous structures [190-196]. It is also noteworthy that mesoporous carbon is also recommended for bacterial adsorption [197]. The application of mesoporous carbon modified electrodes is extended in MFCs, where electron transfer rates have significantly increased [197,198]. Decreasing surface area and increasing pore size and distribution are two morphological parameters that substantially influence macroscale catalytic activity and reactant transport [3]. Activated carbons have surface area over 1000 m²g⁻¹ but are generally unsuitable for supporting biocatalysts because most of this area exists in micropores that are inaccessible to catalysts or even to electrolyte solution [3,199]. In general, enzyme immobilization in nanostructured electrodes extends their lifetime and improves their activity, due to relieved mass transfer limitation of substrates in the nanostructures as compared to macro-scale diffusion, especially when the size of the nanopores is slightly larger than the size of the enzyme.

Metallic oxides and magnetic nanoparticles

Apart from polymers and carbon based materials, oxides and metallic nanomaterials have also been studied extensively for their application in e-BES due to their unique physical and chemical properties [200,201]. Most metallic nanoparticles that have been the focus of research are based on Au, Ag and Pt, due to their high thermal stability, electronic properties and promising applications [200,202]. Similarly, some oxide nanoparticles such as Fe₂O₂, Al₂O₂ and CO₃O₄ [203-205] are well studied in enzymatic fuel cells for valid electron transfer. In comparison with conventional immobilization methods, nanoparticle level immobilization involves three important benefits, viz., ease for synthesis in high solid contents without using surfactants or toxic reagents, homogeneous and well defined structure and distribution can be obtained, and particle size can be conveniently controlled. In addition, with growing attention on multi-enzyme systems, co-immobilization thereof can be achieved in such nanoparticles [206]. Furthermore, magnetic and paramagnetic nanoparticles favor high enzyme-binding capacity and high catalytic specificity along with enhanced stability, due to their surface to volume ratio. Moreover, magnetic nanoparticles can be separated from the reaction medium simply by using a magnet, which was demonstrated in a study with lipase attached to y-Fe₂O₂ nanoparticles by covalent bonds [204]. This allows enzyme reuse over a longer period than that for free or physisorbed enzymes. GOx, peroxidases, β galactosidases, lipases, cholesterol oxidase, trypsine, laccase, a amylase, hemoglobin, cellulase multienzyme mixtures, among others, have also been successfully immobilized (covalently) in this kind of particles, using several ligands. pH, temperature and substrate concentration-stability are also attained for periods as long as three months of continuous operation. Binding efficiency has also shown to increase; moreover, enzyme properties after storage within these particles are also enhanced [206]. Consequently, the use of magnetic nanoparticles represents an innovative approach for enzyme-electrode fabrication without using strong chemicals or high temperatures. Likewise, such particles allow easy-enzyme recovery and reuse which is important for reprocessing, especially when waste or high substrate content streams are considered. Recently, TiO_2 based nanotube arrays, also demonstrated their remarkable charge transfer and photocatalytic properties with enzyme electrodes [207-209]. The application of these novel particles has been demonstrated, as well, in MFCs [205].

Mesoporous and sol-gel based materials

Micellar or mesoporous phases are usually added to the enzyme electrodes to provide an immobilized ion exchanger, buffer, prevent access of poisonous or competitive species, or enhance stability. Such materials are usually polymer or silica-based. Nafion, doped-Nafion, chitosan, have been used on the polymeric approach. In this way reactant permeation is allowed. The process is considered gentle enough that enzymes may be co-casted to form composite membranes [3]. Porous silica structures can encapsulate enzymes by gelation of sol-gel precursors surrounding biomolecules or by adsorption of the enzyme after gelation. The presence of the enzyme restricts the location in which the gel can form [3]. Mobile Crystalline Material MCM-41 (pore size: 4 nm) is a silicate obtained by a templating mechanism, that was the first used for enzyme-electrode immobilization. After it, ordered mesoporous silica (e.g. SBA-15, pore size: 5-13 nm), mesocellular foam (MCF, pore size: 15-40 nm) and mesoporous carbon, have been also applied. Modifications on these materials have also been achieved, such as enlargement of pore size and modified morphologies, for successful enzyme quick adsorption [2]. Sol-gels are porous polymeric matrices with increased surface area which resulted in the development of innovative advanced materials for the immobilization of biological receptors within silica, metal oxide, organosiloxane, and hybrid sol-gel polymers [210-212]. These sol-gel based materials are environmentally friendly and biocompatible and can be combined with many biological systems from molecules to single cells [111]. Sol-gel based materials and their uses for construction of enzyme electrodes have been extensively reported based on their biocompatibility which gives a stable environment for the enzyme function [211,212].

One frequent approach for enzyme immobilization in mesoporous materials is simple adsorption. The stability on the enzymes in such material depends mainly on pore size and charge interaction. It is considered that the pore size of mesoporous materials should be similar to or larger than of enzymes for achieving successful adsorption. The relationship between pore size and molecular diameter is important. Larger pore size, usually leads to poor enzyme stability. If the charge of mesopores is opposite to the net surface charge of the enzymes, it will make a stable system. On the other hand, when the charge is the same, there is repulsion between the enzyme and the surface of mesopores. Charge can be controlled by changing pH, adding buffers or by mesopore functionalization (e.g. with amino or carboxyl groups) [2]. Enzymes covalently attached to mesoporous materials have longer half-life (e.g. 1000 fold higher than that of native enzyme). Beside adsorption and covalent attachment, other approaches can be used for mesoporous material enzyme immobilization, such as partial closure of micropore inlets, nanocomposite shell on the particle surface, and cross-linked enzyme aggregates via a ship-in-a-bottle approach [2].

Ionic liquids

Non-aqueous biocatalytic systems have acquired recent interest because of their unique synthetic opportunities. For example, hydrolytic enzymes (e.g. lipases and esterases) in non-polar, organic solvents with low water content have been shown to carry out reversed hydrolytic and transferase-type reactions in such media. Recently, ionic liquids (ILs) have emerged as an alternative media to non-polar, hydrophobic solvents for supporting biocatalysis [213]. Electrode modification with ILs is interesting due to their hydrophobicity, high viscosity, ionic structure, ionic conductivity, low-volatility and biocompatibility. The electrochemical properties of ionic liquid-modified electrodes (ILME) are determined by the presence of a well-established ionic liquid/liquid interface and three-phase junction electrode/ionic liquid/liquid where in most cases ET starts [214]. Ionic liquids are entirely comprised by anions and cations. A myriad of organic cation and inorganic or organic anion combinations are possible [213,214]. Therefore, the toxicological and pharmacological effects of most ILs have still to be defined. The melting point of most ILs is below room temperature. Their conductivity can be as high as 100 mS cm⁻¹ and bulk electrode materials comprising this liquid acquire this property [215]. Viscosity of ILs is typically in the range of hundreds of mPas (at 25°C). The wide potential window is considered one of the major advantages regarding ILs in electrochemical systems. Indeed, ILs has been used for enzyme electrodes and was reported to increase enzyme stability and activity and for this reason they have become popular as a novel route for enzymeelectrode manufacturing [214]. The presence of specific functionalities in ILs permits their application for electrode modification. For example, the use of amino acid-functionalized IL also provides stable enzyme immobilization [216]. Nonetheless, to date relatively little data exist on the enzymatic activity of oxidoreductases in ILs. Recent studies have shown that the classic redox-active hemoprotein, cytochrome c (cyt-c), and analogues of its active site, conditionally retain peroxidase activity in some ILs, but they must be coordinated with a ligand for this purpose [213].

IL-modified electrodes can be divided into five major categories. 1) Electrodes modified with ionic liquid droplets or films: electrochemically generated ion transfer across IL/aqueous solution interface is observed, and their electrochemical behavior seems more complex than other ILs; however, these ILs produce suitable configuration for enzyme-electrode electron transfer. 2) Film electrodes with ionic liquids as one of the components: they are considered important supports for enzymes, because of its stabilizing properties and because they have supported DET of glucose oxidase, horseradish peroxidase, hemoglobin, myoglobin, cytochrome c, catalase and chloroperoxidase; still, the ET mechanisms with such ILs and enzymes are not yet understood. 3) Carbon paste electrodes with ionic liquid as a binder: they have higher viscosity; complex enzyme-electrode architectures can be built with such ILs.4) Electrodes prepared of ionic liquid-carbon nanotubes gel: GOx has been successfully immobilized in this type of IL-based electrodes; however redox reaction with other enzymes has appeared difficult to achieve, but metallic and magnetic nanoparticles seem an interesting possibility to explore for this type of IL-electrodes. 5) Electrodes modified with appended ionic liquids: contrary to the other ILs presented, these do not consist of the ILs as they are, they are prepared from imidazolium cation ILs with different functionalities related to their immobilization procedure; this is, they are just ionomers with immidazolium functionalities, therefore their wettability can be controlled by electric field. Application of the latter type of ILs to enzyme electrodes has been carried out, however, low current has been observed when compared to bare electrodes, possibly Page 9 of 20

due to ion preconcentration effects [214]. For sure, the presence of ILs affects the ET processes and mechanisms and they bestow numerous unexplored possibilities for enzymatic electrocatalysis.

Composite materials

Apart from all these materials, there are numerous studies based on the combination of two or more kinds of them with resulting significantly different physical or chemical properties. Such materials can be termed as composites. Composite materials have the advantage of combining different structures and their native properties at the macroscopic or microscopic scale [111]. However, they may acquire all the native properties of the different combined materials or may possess unique hybrid properties of neither the incorporated components nor the host matrixes. Though there are several combinations, three major combinations were reported based on immobilization materials by Yang et al. [111]. These include polymer-based composite materials with carbon, nanomaterial and sol-gel, carbon-based composite materials with nanomaterial and sol-gel, and composite of sol-gel materials with metallic oxides and novel nanoparticles [111]. A few examples of these composites include novel metal/CNT/polymer composite electrodes which have presented significantly improved electron transfer properties [217]. Similarly, a new kind of electroactive nanocomposite formed by methylene green, that noncovalently functionalizes chemically reduced graphene, has been applied to e-BES [2,188,189,218-221]. Sol-gel materials incorporating other constituents have also been extensively investigated, with the combinations of biopolymer chitosan [222], CNTs [223], etc. Overall, the combination of two or more compounds can bring some of new properties to the immobilization matrix which helps to support the enzyme activity, stability as well as the electron transfer rates to the electrodes. The incorporation of metallic or semiconductive nanoparticles into conductive polymers can be a typical example, which helps in increasing the electrocatalytic properties of nanoparticles and in return the conductivity of hybrid systems is enhanced with the metal nanoparticles [224].

Electroenzymatic reactions and applications

Enzymatic reactions on electrodes can be applied for anodic oxidation or cathodic reduction reactions, based on its functionality. The enzyme in the anodic compartment oxidizes the substrate, while transferring electrons to the electrically contacted electrode. Similarly, the cathodic enzyme reduces the available oxidizer compound with the help of electrons coming from the anodic oxidation. The electrons will flow through the external circuit, while the protons transfer through the electrolyte. Several enzymes belonging to the family of oxidases and dehydrogenases were studied in fuel cell for anodic oxidation of diverse compounds, for instance, saccharides, alcohols, acids and amino acids, etc. The most studied enzymes at cathode are based on oxygen reduction, such as laccase, peroxidases, etc., [225]. The difference in the thermodynamic redox potentials of the redox enzymes used at anode and cathode, determines the maximum voltage of the biofuel cell. However, the incorporation of redox relays to increase the electrochemical communication between electrodes and enzymes will lead to a potential drop, conducting to lower power outputs. Therefore, it is important to select the mediators with redox potentials close to the thermodynamic potentials of the enzyme. The turnover number of enzyme also plays a crucial role in current generation, which is determined by the rate of reaction occurring between the enzyme and the fuel/oxidizer. Though, two enzymatic electrodes are coupled and operate in a fuel cell, the cathodic reduction reaction is the major rate limiting step determining the current generation, similar to the MFCs. Over 1400 oxidoreductases are known to date (www.enzymedatabase.

org), any of which could possibly be utilized as catalyst in an enzymatic FC. In the majority of cases, the use of mediators is needed to electrically connect the enzyme to the electrode, since only less than about a hundred of the known oxidoreductases are capable to communicate with an electrode surface via a DET mechanism [225]. Many redox enzymes have their catalytic sites buried deeply within the protein matrix, which acts to insulate the redox site and will eventually prevent DET.

Anodic oxidizing reactions: The most studied anodic reactions are based on glucose oxidation using oxidases and dehydrogenases. GOx is a well characterized and stable enzyme studied as anodic biocatalyst of choice for many e-BES [30]. Similarly, the other one is glucose dehydrogenase (GDH), catalyzing a similar reaction, oxidation of glucose to gluconolactone, thereby liberating two electrons. These two enzymes have been studied in the glucose/O₂ system combined with the oxygenases such as laccases, bilirubin oxidases, peroxidases, etc., at the cathode. However, there are numerous other enzymes studied in the e-BES for their catalytic efficiency of oxidation or reduction, which are represented in Table 1.

Indeed, glucose oxidation has been extensively studied in the context of biosensing devices and does not provide a major reaction of interest for industrial exploitation; however, the fundamentals and practical experiences derived from the immoboilization, characterization, analysis and optimization of such enzymatic systems remain important due to their contributions to the overall field of enzymatic electrocatalysis. Apart from the glucose, alcohols were also extensively studied as fuel at anode in e-BES catalyzed by non-specific or specific alcohol dehydrogenases [240,241]. Similarly, cellobiose [229-233], fructose [234,235], pyruvate [227], glycerol [227], hydrogen [238,239], etc., were also studied as fuels in e-BES. Various studies have been performed to enhance the current densities, to meet the complete oxidation of the fuel, to increase the stability and longetivity of the enzyme properties. GOx is a well characterized and stable enzyme which catalyzes the oxidation of glucose to glucanolactone [242]. Several studies were performed to increase the electron transfer in GOx, especially based on using carbon nanotubes (CNTs) and gold nanoparticles [30,36,99,109,156,225,228,243-247], by using mediators such as ferrocene derivatives [59,248,249], by coordination complexes of osmium with polymers [243,250-257], by protein modification and engineering to achieve improved GOx properties [258-260] etc. Likewise, the other enzymes such as GDH, alcohol dehydrogenases were also studied from different sources and with various enhancing strategies in e-BES [14]. Oxidation of H₂ is another potential application in e-BES, where different types of hydrogenases were studied for their function [14,238,239]. [Ni-Fe] hydrogenases with Fe-S cluster were found to be more efficient among these hydrogenases [14]. However, the complete oxidation of any fuel is not feasible in single enzyme catalyzed systems. Few studies on multi-enzyme cascade systems were also reported for the complete oxidation of fuels such as glucose, ethanol, methanol, pyruvate, etc., (see section about Multi enzyme cascades).

Cathodic reduction reactions

Similar to anode, there are several enzymes studied at cathode for completing the reduction reactions. Most of these cathodic enzymes are typically multi-copper oxidases, such as laccases [163], bilirubin oxidase [167], peroxidases [225], etc., which are capable of four-electron O_2 reduction [261]. Laccases are generally employed under slightly acidic conditions, while bilirubin oxidase has its activity in more alkaline media which allows it to be used at neutral pH. Apart from these, several other enzymes such as cytochrome oxidase and cytochrome c, have also been employed at cathodes in e-BES. In the case of H_2O_2 reduction, microperoxidase [99,225] and horseradish peroxidase [262] are commonly used as electrocatalytic enzymes. A comprehensive list enzymes used at cathode in e-BES was depicted in Table 2.

The cathodic reduction reaction is as crucial as anodic oxidation for the completion of the circuit in the electrochemical cell, and needs a terminal electron acceptor, such as oxygen. Various metallic catalysts, such as platinum, have been used to increase both selectivity and electrode kinetics towards reduction reactions at cathodes. However, enzyme-catalyzed cathodes are more efficient [266]. Multiple copper oxidases appear highly relevant in scientific literature, especially laccases, due to their high reduction potential, capacity to utilize multi-atomic reaction sites, flexibility of interatomic distances and the positive influence of residues adjacent to the active site on reaction mechanism [263,267-270]. Laccases from fungal origin are most extensively studied due to the higher redox potential (~0.58 V vs Ag/ AgCl), ligand co-ordination geometry, and the presence of weakly axially co-ordinated residues contributing to the difference in redox potential [30]. However, these fungal laccases are inhibited by hydroxyl ions and, to a lesser extent, by chloride [271], which limits their usage at biocathodes. Apart from this, laccases from plants [263] and bacteria [272,273] have been also studied, but they have a low reduction potential (~0.23 V vs Ag/AgCl). The higher reduction potential of some laccases close to the thermodynamic potential for oxygen reduction enables the effective reduction reaction at cathode. Laccases were adsorbed on graphite [263,274], carbon aerogel, HOPG [183], carbon nanotubes [184,275-277], nanoparticles [278-280], gold nanoparticles [281] to enhance electron transfer rates from laccases. Alternatively,

Enzyme	Substrate/ Fuel	Natural/ Artificial electron acceptor	Co-factor	Half-cell reaction	Reference
Glucose oxidase	Glucose	0 ₂	FAD	Glucose \rightarrow Glucono-1,5lactone+2H ⁺ +2e ⁻	[226-228]
Glucose dehydrogenase	Glucose	NAD	NAD	Glucose → Glucono-1,5lactone+2H ⁺ +2e ⁻	[227]
Glucose dehydrogenase	Glucose	Quinone	PQQ	Glucose → Glucono-1,5lactone+2H ⁺ +2e ⁻	[227]
Cellobiose dehydrogenase	Glucose	FAD	Heme	Glucose \rightarrow Glucono-1,5lactone+2H ⁺ +2e ⁻	[229-232]
	Cellobiose	FAD	Heme	Cellobiose \rightarrow Cellobiono-1,5lactone+2H ⁺ +2e ⁻	[233]
Fructose dehydrogenase	Fructose	FAD	Heme	Fructose \rightarrow 5-dehydrofructose+2H ⁺ +2e ⁻	[234-235
Succinate dehydrogenase	Succinate	FAD	Fe-S	Succinate \rightarrow Fumarate+2H ⁺ +2e ⁻	[236]
Alcohol dehydrogenase	Ethanol	PQQ	Heme	Ethanol → Acetaldehyde+2H ⁺ +2e ⁻	[237]
Oxalate oxidase	Glycerol	0 ₂	FAD,Mn	Oxalate $\rightarrow 2CO_2 + 2H^+ + 2e^-$	[227]
Pyruvate dehydrogenase	Pyruvate	NAD	NAD	Pyruvate+SCoA→acetylCoA+2H ⁺ +2e ⁻	[227]
Hydrogenase	Hydrogen		Fe-S	$H_2 \rightarrow 2H^+ + 2e^-$	[238]
Membrane-bound hydrogenase	Hydrogen		Fe-S	H₂→2H*+2e ⁻	[239]

Table 1: Some of the most studied enzymes for anodic oxidation and their respective reactions.

retention of the enzyme behind a membrane at electrode surface [282] and chemical derivatisation to retain laccase through hydrophobic pockets were also studied to enhance the electron transfer rates [283]. Laccases cross-linked with an osmium-based redox polymer on carbon electrodes were shown to provide steady-state current densities [284]. Bilirubin oxidase [229,231,232] and cytochrome oxidase [285] were studied as alternative to laccases at cathode for O₂ reduction and peroxidases have been well studied for the application in e-BES.

Hydrogen peroxide (H_2O_2) is considered as a stronger oxidant than O_2 at cathode in e-BES which can be oxidized by highly active peroxidases as the cathodic electrocatalyst [286,287]. Horseradish peroxidase, cytochrome c peroxidases and microproxidases are the common peroxidases used in e-BES [19,28,237,262,264]. Apart from these electron acceptors, few other oxidized substrates such as formate, fumerate, aldehydes, etc., were also being studied recently at the cathode of e-BES [54,238,265]. Considering these substrates for their reduction at cathode has opened new windows in the electrosynthesis research where single/multiple enzymes can be used to reduce the unwanted/waste substrates to potential value added products with the help of in situ generated reducing equivalents (H⁺ and e⁻) (see section about Enzymes for electrosynthesis).

Novel enzymes and their applications: Apart from these well studied enzymes, there are several enzymes being studied for their application in the enzymatic electrosynthesis as depicted in the Table 1 and 2. However, certain enzymes should be mentioned here for their novel applications. Peroxidases such as horseradish peroxidase, chloroperoxidase, lignin peroxidase, etc., are well known for their application in treatment of complex and toxic pollutants. For instance, chloroperoxidase has proven highly valuable in the catalysis of epoxidations, hydroxylation, and oxidation of alcohols and indole. Heteroatom oxidation (N- and S- oxidation) has also been achieved; therefore, oxidation of heterocyclic sulfur compounds present in fuels and the modification of petroporphyrins and asphaltene molecules are two promising large-scale applications for e.g. petroleum industry, in order to improve the quality of petroleum and petroleum fuels, as well as for reducing their environmental polluting effects [288]. Studies on this enzyme were also extended to understand DET [215], immobilized on mesoporous materials [288], ionic liquid-modified carbon electrodes [215] and with conductive polymers [289]. Moreover, this enzyme can also be applied at anodes for electrochemical heteroatom oxidation (Nand S⁻ oxidation) with simultaneous cathodic reduction of O₂ and H₂O₂ [215,289].

Multi enzyme cascades: The combination of two or more enzymes

at the anode or cathode as cascade has shown higher anodic oxidation and cathodic reduction reaction rates in e-BES [30,290]. The first and one of the simplest me-BES that have been described is relative to the oxidation of methanol to CO_2 and water by a three-step mechanism catalyzed by NADH-dependent systems [290]. Similarly, the two-step oxidation of ethanol to acetate was also studied in a novel membrane (Nafion) assembly [291]. A polymer-based electrocatalyst (polymethylene green) was used to regenerate NAD⁺ and to shuttle electrons from NADH to the electrode [292].

The complete oxidation of methanol to CO_2 using solution phase dehydrogenases [290] and the reduction of CO_2 to methanol using the enzyme cascade [265] are novel examples of this kind of reactions. Similarly, in some of the studies multi enzyme cascade was used for the complete oxidation of the substrates such as glucose [293], methanol [294], ethanol [295], pyruvate [296-298], glycerol [299-301], etc., to CO_2 generating higher number of electrons. Modified electrodes combining cellobiose dehydrogenase and pyranose dehydrogenase have shown to be capable of extracting up to 6 electrons from one molecule of glucose [302].

The single enzymes in e-BES, studied over the years are, peroxidases, the multicenter redox enzymes hydrogenases, multiheme nitrite reductase, large membrane-bound enzymes including fumarate reductase, succinate dehydrogenases, Mo-containing nitrite reductases, sulfite oxidase and lacasses [72]. The current densities achieved in all these cases are much lower than those achieved by me-BES. Most e-BES implies low efficiency due to single-step redox reactions, but efficiency can be improved by using me-BES. In conclusion, one of the key issues to develop effective and efficient e-BES is the successful immobilization of multi-enzyme systems that can completely oxidize organic compounds to CO_2 or vice versa, in order to increase the overall substrate-to-electrons efficiency of the cell.

Enzymes for electrosynthesis: Electrosynthesis is one of the emerging applications of BES where the negative valued substrates can be converted to commercially viable substrates under small applied potentials in presence of a chemical/biological catalyst. However, biologically catalyzed systems have more significance due to the renewability of the process and recyclability of the catalyst. Several researchers across the globe are currently working on the microbial electrosynthesis process in BES for the production of chemicals and fuels apart from electricity [10-11,303,304]. Bioconversion of fumarate to succinate [305], CO₂ to acetate [306], acetate and butyrate to alcohols, acetone and elongated CFAs such as caproate [1], methane [308,309], volatile acids to polyhydroxyalkanoates [309], etc., have been reported

Enzyme	Oxidizer/ Electron acceptor	Natural/ Artificial electron donor	Co-factor	Half-cell reaction	Reference
Laccase	0 ₂		Cu	O ₂ +4H⁺+4e ⁻ →2H ₂ O	[226,228,239,263]
Bilirubin oxidase	0 ₂		Cu	O ₂ +4H⁺+4e ⁻ →2H ₂ O	[229,231-232]
Chloroperoxidase	H ₂ O ₂		Heme	$H_2O_2+2H^++2e^-\rightarrow 2H_2O$	[21]
Cytochrome c peroxidase	H ₂ O ₂		Heme	$H_2O_2+2H^++2e^-\rightarrow 2H_2O$	[19]
Microperoxidase	H ₂ O ₂		Heme	$H_2O_2+2H^++2e^-\rightarrow 2H_2O$	[28,237,264]
Horseradish peroxidase	H ₂ O ₂		Heme	$H_2O_2+2H^++2e^-\rightarrow 2H_2O$	[262]
Fumarate reductase	Fumarate	FAD	Fe-S	Fumarate+2H ⁺ +2e ⁻ \rightarrow Succinate	[264]
Alcohol dehydrogenase	Formaldehyde	Neutral red	NAD	Formaldehyde+2H ⁺ +2e ⁻ \rightarrow Methanol	[265]
Formaldehyde dehydrogenase	Formate	Neutral red	NAD	Formate + $2H^++2e^- \rightarrow$ Formaldehyde + H_2O	[265]
Formate dehydrogenase	HCO ³⁻	Neutral red	NAD	$HCO^{3-}+2H^++2e^- \rightarrow Formate$	[265]
Carbonic anhydrase	CO2	Neutral red		$CO_2 + H_2O \rightarrow HCO^{3-} + H^+$	[265]
Hydrogenase	H ⁺	Methyl viologen	Fe-S	$2H^++2e^- \rightarrow H_2$	[238]

Table 2: Some of the most studied enzymes for cathodic reduction and their respective reactions.

so far. Still further research is on and going towards the production of various commercially viable products in renewable and sustainable way through BES. On the contrary, the research in the direction of enzymatic electrosynthesis has started more recently and very few articles are available in the literature. The major hurdles in this area is requirement of single substrate, stability and longetivity of enzymes, interference reactions, end-product inhibition, etc. Recent report on the methanol production from CO₂ [265], has shown the possibility of using CO₂ as precursor for the synthesis of useful chemicals and fuels at cathode in e-BES. Various novel routes for the product synthesis through enzymatic/chemo-enzymatic processes were reported extensively [310]. Adapting these enzymatic processes at e-BES cathode will have an added advantage of simultaneous power generation and co-factor regeneration. Electrosynthesis of methanol, ethanol, butanol, acetate, fumerate, etc., using enzymes cascades should be focused. Similarly, the conversion of waste glycerol, a major intermediate from biodiesel industry [310], to dihydroxyacetone phosphate, synthesis of polyhydroxyalkanoates using volatile acid straems also has higher commercial viability.

Criteria and cost elements for industrial processing with e-BES

According to the state of the art literature, industrial biotransformations must minimally consider three key factors:1) product yield (gram product per gram substrate/enzyme), 2) product titer (gram product per liter), and productivity (gram product per liter per hour) [8]. However, electrochemically-mediated enzymatic processes and biological in general—must be seen from additional perspectives, due to their heterogeneous-catalytic nature. Current density (amperes per square meter of electrode), faradic efficiency or fuel utilization efficiency (% of substrate to electrons conversion, from bioelectrochemical reactions) and energy efficiency (useful power output per total power input), are other core parameters related to production within these systems.

Product yield and faradic efficiency are considered the most important for the production of biocommodities by e-BES, since a large fraction (30-70%) of the conversion step costs come from feedstock [8]. Product titer and current density come next in importance. Especially high-value products are habitually present in rather diluted concentrations and require intensive separations. Besides, reduced quantities are obtained from large electrode surfaces, which represent a significant extent of the processing costs [8]. Product yield is not significant for final product production costs. However, energy efficiency becomes important when enzymatic electrolysis or electrosynthesis are anticipated, since generally about 70-80% of the costs in electrochemical processing account for electricity [311,312].

In their application as enzymatic fuel cells, e-BES must have a positive energy budget. This is the power relative to consumption, i.e. pumping, must be lower compared to the power output from the electrochemical cell. In addition, especially if such enzymatic power source is meant to be applied as implantable or portable power source, economy of scale becomes highly relevant for comparison to batteries, as the latter have no pumping costs and relies only on diffusion. Volume and weight become critical for such comparison [313].

Compared to metallic electrocatalysts, enzymatic electrocatalysts offer competitive advantages. For instance, since biocatalysts are nowadays produced industrially, production costs are rather low, while this is opposite for the case of transition metal catalysts [313]. Still, there is further work needed to understand important enzymatic and engineering issues, especially when scale-up for industrial bioproduction is foreseen. So far, for such applications, there are no electroenzymatic pilot studies available. For this reason, scaled-up demonstration projects are required in order to prove the reliability and cost-effectiveness of enzymatic electrocatalysis. Although initially enzymatic electrocatalysis has evolved in the context of biosensors and now it has been moving to the field of miniaturized power devices, it is likely that it finds soon an industrial niche on the synthesis of fuels and chemicals as well. Given that electricity costs are relatively low compared with the value of such product chemicals, enzymatic electrosynthesis will become a key process for chemical synthesis if lifetime of enzymatic electrodes and reactor engineering issues are soon overcome.

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On the other hand, enzymatic systems involve additional costs associated to their production. Specifically, separation and stabilization costs, as well as addition of coenzymes, are critical factors. For example, the cost factor to purify stabilized enzymes aimed for sugar oxidation $(C_{\rm p})$ can be calculated as [8]:

$C_{E} = F_{M} C_{S} F_{P} F_{S} / Y_{X/S}^{E} Y_{E/X}$

Where $\rm F_{M}$ is a cost correction coefficient for fermentation relative to sugar, $\rm C_{S}$ is the cost of sugar (\$ per kg of sugar), FP and FS are coefficients concerning the ratio between pure and crude enzyme and stabilized to free enzyme, respectively. $\rm Y_{E/X}$ is the yield of desired enzyme based on microbe mass (kg enzyme per kg cell mass). $\rm Y^{E}_{X/S}$ is the cell mass yield, based on sugar (kg cell mass per kg sugar), being 0.5 for aerobic fermentations for the production of the desired enzymes. Processes for enzyme overproduction typically haave have values of $\rm Y_{E/X}$ ranging from 0.1 to 0.4 [8].

The total enzymatic turnover based on product weight (TTN_w) is also an important parameter, especially when compared to microbial electrocatalytic systems. The TTNW is typically 1 to 7 orders of magnitude higher for enzymatic systems than for microbial systems [8]. This can be extrapolated to enzymatic electrocatalytic systems, as they have higher reaction specificity and due to their possibility of direct electron transfer when immobilized which also confers longerterm stability as compared to free enzymes.

Of course, the development of ready-to-use and stable low-cost enzyme electrodes is anticipated to become the most critical factor in order to enable enzymatic electrocatalysis for bioproduction at industrial level. The research group oject of the present review is taking pioneering actions in this direction, being one of the leading groups in the fabrication and optimization of good performing electrodes for microbial electrochemical and classical electrochemical systems [1,155,314].

Conclusion

Though the concept of enzyme catalysis has existed since long time, its potential in the production of bioelectricity and biocommodities has recently emerged due to the discovery of bioelectrochemical systems (out of the biosensor applications). Some major bottlenecks that could hinder its industrial application are: the lack of long-term stability of single and multi-enzyme systems, non-uniform enzyme distribution on enzyme-electrodes, aggressive manufacturing procedures (pH, T, strong chemicals), inefficient electron transfer due to enzyme-electrode weak contact, reactant interference and contaminants which leads to the low productivity, current density and coulombic efficiencies. Enzymatic electrosynthesis and paired electrolysis are barely explored fields that offer a chance for industrial innovation towards green

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chemistry applications. Success in this direction strongly depends on the advancement made in the enzyme immobilization methods, as well as on the right choices on enzymes, target reactions, materials and composites. Composites with performing electrode material and ionic liquids, magnetic nanoparticles, carbon nanotubes or mesoporous materials seem promising approaches for increasing the enzyme to electrode wiring potential.

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References

- Sharma M, Aryal N, Sarma PM, Vanbroekhoven K, Lal B, et al. (2013) Bioelectrocatalyzed reduction of acetic and butyric acids via direct electron transfer using a mixed culture of sulfate-reducers drives electrosynthesis of alcohols and acetone. Chem Commun (Camb) 49: 6495-6497.
- Kim J, Jia H, Wang P (2006) Challenges in biocatalysis for enzyme-based biofuel cells. Biotechnol Adv 24: 296-308.
- Barton SC (2010) Enzyme catalysis in biological fuel cells: Handbook of Fuel Cells. John Wiley & Sons, Ltd.
- Kohlmann C, Märkle W, Lütz S (2008) Electroenzymatic synthesis. J Mol Cat B: Enz 51: 57-72.
- 5. Bard AJ, Stratmann M (2002) Encyclopedia of Electrochemistry: Bioelectrochemistry Wiley-VCH.
- 6. Yu EH, Scott K (2010) Enzymatic biofuel cells-Fabrication of enzyme electrodes. Energies 3: 23-42.
- Rabaey K, Angenent L., Schroder U., Keller J. (2009) Bioelectrochemical systems: from extracellular electron transfer to biotechnological application. (1st ed.) IWA Publishing, Lodon (2009).
- Zhang YH (2010) Production of biocommodities and bioelectricity by cell-free synthetic enzymatic pathway biotransformations: challenges and opportunities. Biotechnol Bioeng 105: 663-677.
- Schröder U (2007) Anodic electron transfer mechanisms in microbial fuel cells and their energy efficiency. Phys Chem Chem Phys 9: 2619-2629.
- Mohan SV, Srikanth S, Velvizhi G, Babu ML (2013) Microbial fuel cells for sustainable bioenergy generation: principles and perspective applications (Chapter 11): Biofuel Technologies: Recent Developments Gupta VK, Tuohy MG, (Eds) Spinger.
- 11. Rabaey K, Rozendal RA (2010) Microbial electrosynthesis revisiting the electrical route for microbial production. Nat Rev Microbiol 8: 706-716.
- Habermüller K, Mosbach M, Schuhmann W (2000) Electron-transfer mechanisms in amperometric biosensors. Fresenius J Anal Chem 366: 560-568.
- Ferapontova EE, Shleev S, Ruzgas T, Stoica L, Christenson A, et al. (2005) Direct electrochemistry of proteins and enzymes: Perspectives in Bioanalysis, Paleiek FSE (Ed) 1-81.
- Cracknell JA, Vincent KA, Armstrong FA (2008) Enzymes as working or inspirational electrocatalysts for fuel cells and electrolysis. Chem Rev 108: 2439-2461.
- Barton SC, Gallaway J, Atanassov P (2004) Enzymatic biofuel cells for implantable and microscale devices. Chem Rev 104: 4867-4886.
- Ludwig R, Harreither W, Tasca F, Gorton L (2010) Cellobiose dehydrogenase: a versatile catalyst for electrochemical applications. Chemphyschem 11: 2674-2697.
- Christenson A, Dimcheva N, Ferapontova EE, Gorton L, Ruzgas T, et al. (2004) Direct electron transfer between ligninolytic redox enzymes and electrodes. Electroanal 16: 1074-1092.
- Shleev S, Tkac J, Christenson A, Ruzgas T, Yaropolov AI, et al. (2005) Direct electron transfer between copper-containing proteins and electrodes. Biosens Bioelectron 20: 2517-2554.
- 19. Armstrong FA, Lannon AM (1987) Fast interfacial electron-transfer

between cytochrome-c peroxidase and graphite-electrodes promoted by aminoglycosides - novel electroenzymic catalysis of $\rm H_2O_2$ reduction. J Am Chem Soc 109:7211–7212.

- Yaropolov AJ, Malovik V, Varfolomeev SD, Berezin IV (1979) Doklady AN USSR 249: 1399–1401.
- Ruzgas T, Gorton L, Emnéus J, Csöregi E, Marko-Varga G (1995) Direct bioelectrocatalytic reduction of hydrogen-peroxide at chloroperoxidase modified graphite electrode. Anal Proc 32: 207-208.
- Ruzgas T, Csöregi E, Emneus J, Gorton L, Marko-Varga G (1996) Peroxidasemodified electrodes: Fundamentals and application. Anal Chim Acta 330: 123–138.
- Ferri T, Poscia A, Santucci R (1998) Direct electrochemistry of membraneentrapped horseradish peroxidase. Part II: Amperometric detection of hydrogen peroxide. Bioelectrochem Bioenerg 45: 221–226.
- 24. Lindgren A, Munteanu FD, Gazaryan I, Ruzgas T, Gorton L(1998) Comparison of rotating disk and wall-jet electrode systems for studying the kinetics of direct and mediated electron transfer for horseradish peroxidase on a graphite electrode. J Electroanal Chem 458 :113–120.
- Kulys J, Schmid RD (1990) Mediatorless peroxidase electrode and preparation of bienzyme sensors. Bioelectrochem Bioenerg 24: 305–311.
- Wollenberger U, Wang J, Ozsoz M, Gonzalez-Romero E,Scheller F (1991) Bulk modified enzyme electrodes for reagentless detection of peroxides. Bioelectrochem Bioenerg 26: 287–296.
- Csöregi E, Jönsson-Petterson G, Gorton L (1993) Mediatorless electrocatalytic reduction of hydrogen-peroxide at graphite-electrodes chemically-modified with peroxidases. J Biotechnol 30 :315–317
- Razumas V, Kazlauskaite J, Ruzgas T, Kulys J (1992) Bioelectrochemistry of microperoxidases. Bioelectrochem Bioenerg 28: 159–176.
- Ghindilis AL, Atanasov P, Wilkins E (1997) Enzyme-catalyzed direct electron transfer: Fundamentals and analytical applications. Electroanal 9: 661-674.
- Leech D, Kavanagh P, Schuhmann W (2012) Enzymatic fuel cells: Recent progress. Electrochim Acta 84: 223–234.
- Marcus RA, Sutin N (1985) Electron transfers in chemistry and biology. Biochim Biophys Acta 811: 265–322.
- 32. Marcus RA (1993) Electron-transfer reactions in chemistry theory and experiment (nobel lecture). Angew Chem Int Ed English 32: 1111–1121
- Karyakin AA, Karyakina EE, Schuhmann W, Schmidt HL, Varfolomeyev SD (1994) New amperometric dehydrogenase electrodes based on electrocatalytic nadh-oxidation at poly(methylene blue)-modified electrodes. Electroanal 6: 821–829.
- Ferapontova EE (2006) Unmediated enzyme electrodes: Encyclopedia of sensors. Grimes CA, Dickey EC, Pushko MV (Ed) American scientific publishers. 10: 391-421.
- Lötzbeyer T, Schuhmann W, Schmidt HL, Eugenii K, Josef Falter (1994) Direct electron-transfer between the covalently immobilized enzyme microperoxidase mp-11 and a cystamine-modified gold electrode. J Electroanal Chem 377:291– 294.
- Willner I, Helegshabtai V, Blonder R, Katz E, Tao GL (1996) Electrical wiring of glucose oxidase by reconstitution of FAD-modified monolayers assembled onto Au-electrodes. J Am Chem Soc 118: 10321–10322.
- CocheGuerente L, Cosnier S, Labbe L (1997) Sol-gel derived composite materials for the construction of oxidase/peroxidase mediatorless biosensors. Chem Mater 9:1348–1352.
- Dupoet P, Miyamoto S, Murakami T, Kimura J, Karubel (1990) Direct electrontransfer with glucose-oxidase immobilized in an electropolymerized poly(nmethylpyrrole) film on a gold microelectrode. Anal Chim Acta 235: 255-263.
- Koopal CGJ, De Ruiter B, Nolte RJM (1991) Amperometric biosensor based on direct communication between glucose-oxidase and a conducting polymer inside the pores of a filtration membrane. J Chem Soc-Chem Commun 1691– 1692.
- Koopal CGJ, Bos AACM, Nolte RJM (1994) 3rd-Generation glucose biosensor incorporated in a conducting printing ink. Sens Actuators B 18: 166–170.
- 41. Vanos PJHJ, Bult A, Koopal CGJ, Vanbennekom WP (1996) Glucose detection

Page 14 of 20

at bare and sputtered platinum electrodes coated with polypyrrole and glucose oxidase. Anal Chim Acta 335: 209–216.

- 42. Bartlett PN, Birkin PR, Palmisano F, De Benedetto G (1996) A study on the direct electrochemical communication between horseradish peroxidase and a poly(aniline) modified electrode. J Chem Soc Faraday Trans 92: 3123–3130.
- Yabuki S, Shinohara H, Aizawa M (1989) Electro-conductive enzyme membrane. J Chem Soc Chem Commun 945–946.
- Belanger D, Nadreau J, Fortier G (1989) Electrochemistry of the polypyrrole glucose-oxidase electrode. J Electroanal Chem 274: 143–155.
- Cooper JM, Bloor D (1993) Evidence for the functional mechanism of a polypyrrole glucose-oxidase electrode. Electroanal 5: 883–886.
- 46. Ramanavicius A, Habermuller K, Csöregi E, Laurinavicius V, Schuhmann W (1999) Polypyrrole-entrapped quinohemoprotein alcohol dehydrogenase. Evidence for direct electron transfer via conducting-polymer chains. Anal Chem 71: 3581-3586.
- Khan GF, Shinohara H, Ikariyama Y, Aizawa M (1991) Electrochemicalbehavior of monolayer quinoprotein adsorbed on the electrode surface. J Electroanal Chem 315: 263–273.
- Ikeda T (1997) Frontiers in Biosensors I: Fundamental Aspects. Scheller FW, Schubert F, Fedrowitz J, (Ed) Birkhäuser, Basel.
- Ikeda T, Matsushita M, Senda M (1991) Amperometric fructose sensor based on direct bioelectrocatalysis. Biosens Bioelectron 6:299–304.
- Ikeda T, Miyaoka S, Matsushita F, Kobayashi D, Senda M (1992) Direct bioelectrocatalysis at metal and carbon electrodes modified with adsorbed D-gluconate dehydrogenase or adsorbed alcohol-dehydrogenase from bacterial-membranes. Chem Lett 5: 847–850.
- Ikeda T, Miyaoka S, Miki K (1993) Enzyme-catalyzed electrochemical oxidation of d-gluconate at electrodes coated with d-gluconate dehydrogenase, a membrane-bound flavohemoprotein. J Electroanal Chem 352: 267–278.
- Guo LH, Hill HAO, Lawrence GA, Sanghera GS, Hooper DJ (1989) Direct unmediated electrochemistry of the enzyme para-cresolmethylhydroxylase. J Electroanal Chem 266: 379–396.
- Guo LH, Hill HA, Hopper DJ, Lawrance GA, Sanghera GS (1990) Direct voltammetry of the Chromatium vinosum enzyme, sulfide:cytochrome c oxidoreductase (flavocytochrome c552). J Biol Chem 265: 1958-1963.
- 54. Sucheta A, Cammack R, Weiner J, Armstrong FA (1993) Reversible electrochemistry of fumarate reductase immobilized on an electrode surface direct voltammetric observations of redox centers and their participation in rapid catalytic electron-transport. Biochem 32: 5455–5465.
- 55. Larsson T, Elmgren M, Lindquist SE, Tessema M, Gorton L, Henriksson G (1996) Electron transfer between cellobiose dehydrogenase and graphite electrodes. Anal Chim Acta 331: 207–215.
- Liedberg B, Yang Z, Engquist I, Wirde M, Gelius U, et al (1997) Self-assembly of alpha-functionalized terthiophenes on gold. J Phys Chem B 101:5951–5962.
- 57. Chaubey A, Malhotra BD (2002) Mediated biosensors. Biosens Bioelectron 17: 441-456.
- Kulys JJ, Samalius AS, Svirmickas GJ (1980) Electron exchange between the enzyme active center and organic metal. FEBS Lett 114: 7-10.
- Cass AE, Davis G, Francis GD, Hill HA, Aston WJ, et al. (1984) Ferrocenemediated enzyme electrode for amperometric determination of glucose. Anal Chem 56: 667-671.
- Cekic SZ, Holtmann D, Güven G, Mangold KM, Schwaneberg U, et al (2010) Mediated electron transfer with P450cin. Electrochem Comm 12: 1547-1550.
- Schläpfer P, Mindt W, Racine P (1974) Electrochemical measurement of glucose using various electron acceptors. Clin Chim Acta 57: 283-289.
- Kulys JJ, Cenas NK (1983) Oxidation of glucose-oxidase from penicillium-vitale by one-electron and 2-electron acceptors. Biochim Biophys Acta 744 :57–63.
- Cass AEG, Davis G, Green MJ, Hill HAO (1985) Ferricinium ion as an electronacceptor for oxido-reductases. J Electroanal Chem 190: 117–127.
- Yokoyama K, Tamiya E, Karube I (1989) Kinetics of an amperometric glucose sensor with a soluble mediator. J Electroanal Chem 273: 107–117.
- Koudelka M, Gernet S, De Rooij NF (1989) Planar amperometric enzymebased glucose microelectrode. Sens Act B Chem 18:157–165.

- Thornton AJ, Brown DE (1991) Fermentation glucose assay using the exactech blood-glucose biosensor. Biotechnol Tech 5 :363–366.
- Battaglini F, Calvo EJ (1994) Enzyme catalysis at hydrogel-modified electrodes with soluble redox mediator. J Chem Soc, Farad Transact 90:987-995.
- Claremont DJ, Sambrook IE, Penton C, Pickup JC (1986) Subcutaneous implantation of a ferrocene-mediated glucose sensor in pigs. Diabetologia 29: 817-821.
- Jönsson G, Gorton L, Pettersson L (1989) Mediated electron transfer from glucose oxidase at a ferrocene-modified graphite electrode. Electroanal 1: 49–55.
- Brooks SL, Turner APF (1987) Biosensors for measurement and control. Measur Cont 20: 3743.
- Schuhmann W, Lammert R, Uhe B, Schmidt H-L (1990) Polypyrrole, a new possibility for covalent binding of oxidoreductases to electrode surfaces as a base for stable biosensors. Sens Act B Chem 1:537–541.
- Zhang J, Kuznetsov AM, Medvedev IG, Chi Q, Albrecht T, et al. (2008) Singlemolecule electron transfer in electrochemical environments. Chem Rev 108: 2737-2791.
- Schuhmann W (1995) Electron-transfer pathways in amperometric biosensors. Ferrocene-modified enzymes entrapped in conducting-polymer layers. Biosens Bioelectron 10:181–193.
- Matuszewski W, Trojanowicz M (1988) Graphite paste-based enzymatic glucose electrode for flow injection analysis. Anal 113:735-738.
- 75. Pandey PC (1998) Enzyme and microbial biosensors. Humana Press, Totowa, NJ, USA
- Senda M, Ikeda T, Hiasa H, Miki K (1986) Amperometric biosensors based on a biocatalyst electrode with entrapped mediator. Anal Sci 2 : 501–506.
- Dicks JM, Aston WJ, Davis G, Turner APF (1986) Mediated amperometric biosensors for d-galactose, glycolate and l-amino acids based on a ferrocenemodified carbon paste electrode. Anal Chim Acta 182:103–112.
- Wang J, Wu L-H, Lu Z, Li R, Sanchez J (1990) Mixed ferrocene-glucose oxidase-carbon-paste electrode for amperometric determination of glucose. Anal Chim Acta 228:251–257.
- 79. Kulys J, Schuhmann W, Schmidt HL (1992) Carbon-paste electrodes with incorporated lactate oxidase and mediators. Anal Lett 25 : 1011–1024.
- Kacaniklic V, Johansson K, Marko-Varga G, Gorton L, Jönsson-Pettersson G, Csöregi E (1994) Amperometric biosensors for detection of L- and D-amino acids based on coimmobilized peroxidase and L- and D-amino acid oxidases in carbon paste electrodes. Electroanal 6:381–390.
- Hedenmo M, Narváez A, Domínguez E, Katakis I (1997) Improved mediated tyrosinase amperometric enzyme electrodes. J Electroanal Chem 425:1–11.
- Baldwin RP, Thomsen KN (1991) Chemically modified electrodes in liquid chromatography detection: A review. Talanta 38: 1-16.
- Brown RS, Luong JHT (1995) A regenerable pseudo-reagentless glucose biosensor based on Nafion polymer and I,1'-dimethylferricinium mediator. Anal Chim Acta 310:419–427.
- 84. Liu H, Ying T, Sun K, Li H, Qi D (1997) Reagentless amperometric biosensors highly sensitive to hydrogen peroxide, glucose and lactose based on N-methyl phenazine methosulfate incorporated in a Nafion film as an electron transfer mediator between horseradish peroxidase and an electrode. Anal Chim Acta 344:187–199.
- Viallancourt M, Chen JW, Fortier G, Belanger D (1999) Electrochemical and enzymatic studies of electron transfer mediation by ferrocene derivatives with Nafion-glucose oxidase electrodes. Electroanal 11:23–31.
- Lei C, Zhang Z, Liu H, Deng J (1996) Studies on employing tetrathiafulvalene as an electron shuttle incorporated in a montmorillonite-modified immobilization matrix for an enzyme electrode. J Electroanal Chem 419:93–98.
- Wang J, Varughese K (1990) Polishable and robust biological electrode surfaces. Anal Chem 62: 318-320.
- Kotte H, Gruendig B, Vorlop K-D, Strehlitz B, Stottmeister U (1995) Methylphenazonium-modified enzyme sensor based on polymer thick films for subnanomolar detection of phenols. Anal Chem 67:65–70.
- 89. Lange MA, Chambers JQ (1985) Amperometric determination of glucose with a

ferrocene-mediated glucose oxidase/polyacrylamide gel electrode. Anal Chim Acta 175:89–97.

- Iwakura C, Kajiya Y, Yoneyama H (1988) Simultaneous immobilization of glucose oxidase and a mediator in conducting polymer films. J Chem Soc, Chem Comm 15:1019-1020.
- Bartlett PN, Ali Z, Eastwick-Field V (1992) Electrochemical immobilisation of enzymes Part 4-Co-immobilisation of glucose oxidase and ferro/ferricyanide in poly(N-methylpyrrole) films. J Chem Soc, Farad Transact 88:2677-2683.
- Schuhmann W, Ohara TJ, Schmidt HL, Heller A (1991) Electron transfer between glucose oxidase and electrodes via redox mediators bound with flexible chains to the enzyme surface. J American Chem Soc 113:1394–1397.
- Ryabov AD, Trushkin AM, Baksheeva LI, Gorbatova RK, Kubrakova IV, et al (1992) Chemical attachment of organometallics to proteins in reverse micelles. Angew Chem Int ed Eng 31:789–790.
- 94. Tsai W-C, Cass AEG (1995) Ferrocene-modified horseradish peroxidase enzyme electrodes. A kinetic study on reactions with hydrogen peroxide and linoleic hydroperoxide. Analyst 120:2249-2254.
- Ryabova ES, Goral VN, Csöregi E., Mattiasson B., Ryabov AD (1999) Coordinative approach to mediated electron transfer: Ruthenium complexed to native glucose oxidase. Angew Chem Int Ed Engl 38: 804–807.
- 96. Degani Y, Heller A (1987) Direct electrical communication between chemically modified enzymes and metal electrodes. I. Electron transfer from glucose oxidase to metal electrodes via electron relays, bound covalently to the enzyme. J Phys Chem B 91:1285–1289.
- Bartlett PN, Whitaker RG, Green MJ, Frew J (1987) Covalent binding of electron relays to glucose oxidase. J Chem Soc, Chem Comm 20:1603-1604.
- Sampath S, Lev O (1996) Renewable, reagentless glucose sensor based on a redox modified enzyme and carbon-silica composite. Electroanal 8:1112–1116.
- Katz E, Riklin A, Heleg-Shabtai V, Willner I, Bückmann AF (1999) Glucose oxidase electrodes via reconstitution of the apo-enzyme: tailoring of novel glucose biosensors. Anal Chim Acta 385:45–58.
- 100. Campas i Homs M (2003) Functional oligonucleotide recognition nanomodules for electrochemical DNA biosensors. Spain, Universitat Rovira i Virgili.
- 101. Thomasset B, Thomasset T, Vejux A, Jeanfils J, Barbotin J-N, Thomas D (1982) Immobilized thylakoids in a cross-linked albumin matrix: Effects of cations studied by electron microscopy, fluorescence emission, photoacoustic spectroscopy, and kinetic measurements. Plant Physiol 70:714–722.
- 102. Meunier CF, Yang X-Y, Rooke JC, Su B-L (2011) Biofuel cells based on the immobilization of photosynthetically active bioentities. ChemCatChem 3:476– 488.
- 103. Jochems P, Satyawali Y, Diels L, Dejonghe W (2011) Enzyme immobilization on/in polymeric membranes: status, challenges and perspectives in biocatalytic membrane reactors (BMRs). Green Chem 13:1609-1623.
- 104. Shuler ML, Hallsby GA, Pyne JW, Cho T (1986) Bioreactors for immobilized plant cell cultures. Ann NY Acad Sci 469:270–278.
- 105. Dörnenburg H, Knorr D (1995) Strategies for the improvement of secondary metabolite production in plant cell cultures. Enz Microbial Technol 17:674–684.
- 106.Nguyen QT, Glinel K, Pontié M, Ping Z (2004) Immobilization of biomacromolecules onto membranes via an adsorbed nanolayer. J Mem Sci 232:123–132.
- 107. Costa F, Carvalho IF, Montelaro RC, Gomes P, Martins MC (2011) Covalent immobilization of antimicrobial peptides (AMPs) onto biomaterial surfaces. Acta Biomater 7: 1431-1440.
- 108. Cosnier S (2000) Biosensors based on immobilization of biomolecules by electrogenerated polymer films. New perspectives. Appl Biochem Biotechnol 89: 127-138.
- 109.Willner I, Yan Y-M, Willner B, Tel-Vered R (2009) Integrated enzyme-based biofuel cells-A review. Fuel Cells 9:7–24.
- Osman MH, Shah AA, Walsh FC (2011) Recent progress and continuing challenges in bio-fuel cells. Part I: enzymatic cells. Biosens Bioelectron 26: 3087-3102.
- 111. Yang XY, Léonard A, Lemaire A, Tian G, Su BL (2011) Self-formation phenomenon to hierarchically structured porous materials: design, synthesis,

formation mechanism and applications. Chem Commun (Camb) 47: 2763-2786.

- 112. Xiao Y, Patolsky F, Katz E, Hainfeld JF, Willner I (2003) "Plugging into Enzymes": nanowiring of redox enzymes by a gold nanoparticle. Science 299: 1877-1881.
- 113. Katz E, Willner I (2004) Integrated nanoparticle-biomolecule hybrid systems: synthesis, properties, and applications. Angew Chem Int Ed Engl 43: 6042-6108.
- 114. Zhao J, O'Daly JP, Henkens RW, Stonehuerner J, Crumbliss AL (1996) A xanthine oxidase/colloidal gold enzyme electrode for amperometric biosensor applications. Biosens Bioelectron 11:493–502.
- 115. Bharathi S, Nogami M (2001) A glucose biosensor based on electrodeposited biocomposites of gold nanoparticles and glucose oxidase enzyme. Analyst 126: 1919-1922.
- 116. Wang XY, Zhong H, Lv Y, Chen HY (2003) Fabrication of Nanoelectrode Ensembles of Porous Gold Nanoshells and Direct Electrochemistry of Horseradish Peroxidase Immobilized on the Electrode. Chem Let 32:1054– 1055.
- 117. Liu S, Ju H (2003) Reagentless glucose biosensor based on direct electron transfer of glucose oxidase immobilized on colloidal gold modified carbon paste electrode. Biosens Bioelectron 19: 177-183.
- 118. Liu T, Zhong J, Gan X, Fan C, Li G, et al. (2003) Wiring electrons of cytochrome c with silver nanoparticles in layered films. Chemphyschem 4: 1364-1366.
- 119. Liu S, Dai Z, Chen H, Ju H (2004) Immobilization of hemoglobin on zirconium dioxide nanoparticles for preparation of a novel hydrogen peroxide biosensor. Biosens Bioelectron 19: 963-969.
- 120.Wang L, Erkang Wang (2004) A novel hydrogen peroxide sensor based on horseradish peroxidase immobilized on colloidal Au modified ITO electrode. Electrochem Comm 6:225–229.
- 121.Zhang Y, He P, Hu N (2004) Horseradish peroxidase immobilized in TiO2 nanoparticle films on pyrolytic graphite electrodes: direct electrochemistry and bioelectrocatalysis. Electrochim Acta 49:1981–1988.
- 122. Han X, Cheng W, Zhang Z, Dong S, Wang E (2002) Direct electron transfer between hemoglobin and a glassy carbon electrode facilitated by lipidprotected gold nanoparticles. Biochim Biophys Acta (BBA) - Bioenerg 1556:273–277.
- 123. An J, Jeon H, Lee J, Chang IS (2011) Bifunctional silver nanoparticle cathode in microbial fuel cells for microbial growth inhibition with comparable oxygen reduction reaction activity. Environ Sci Technol 45: 5441-5446.
- 124. Reneker DH, Chun I (1996) Nanometre diameter fibres of polymer, produced by electrospinning. Nanotechnol 7:216–223.
- 125. MacDiarmid AG, Jones WE, Norris ID, et al (2001) Electrostatically-generated nanofibers of electronic polymers. Syn Met 119:27–30.
- 126. Megelski S, Stephens JS, Chase DB, Rabolt JF (2002) Micro- and nanostructured surface morphology on electrospun polymer fibers. Macromolecul 35:8456–8466.
- 127. Frenot A, Chronakis IS (2003) Polymer nanofibers assembled by electrospinning. Curr Opin Coll Int Sci 8:64–75.
- Wnek GE, Carr ME, Simpson DG, Bowlin GL (2003) Electrospinning of nanofiber fibrinogen structures. Nano Lett 3:213–216.
- 129.Li D, Xia Y (2004) Direct fabrication of composite and ceramic hollow nanofibers by electrospinning. Nano Lett 4:933–938.
- 130.Sakai S, Antoku K, Yamaguchi T, Kawakami K (2008) Development of electrospun poly(vinyl alcohol) fibers immobilizing lipase highly activated by alkyl-silicate for flow-through reactors. J Mem Sci 325: 454-459.
- 131.Jia H, Zhu G, Vugrinovich B, Kataphinan W, Reneker DH, et al. (2002) Enzyme-carrying polymeric nanofibers prepared via electrospinning for use as unique biocatalysts. Biotechnol Prog 18: 1027-1032.
- 132.Dabney S, Kataphinan W, Reneker D, Smith D (2002) Preservation of biological materials using fiber-forming techniques. WO 2002100628.
- 133.Xie J, Hsieh YL (2003) Ultra-high surface fibrous membranes from electrospinning of natural proteins: casein and lipase enzyme. J Mater Sci 38: 2125–2133.

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- 134.Bruno FF, Drew C, Nagarajan R, Wang X, Kumar J, Samuelson LA (2004) Conductive polymer complexes from macromolecule inspired biocatalysis. Polym Mater Sci Eng 90: 234–235.
- 135. Cecile C, Chen H, Hsieh Y-L, Li L, Wang Y, et al (2004) Nano-porous fibers and protein membranes PCT Int Appl WO 2004044281.
- 136. Chua KN, Lim WS, Zhang P, Lu H, Wen J, et al. (2005) Stable immobilization of rat hepatocyte spheroids on galactosylated nanofiber scaffold. Biomaterials 26: 2537-2547.
- 137. Chen S, Hou H, Harnisch F, et al (2011) Electrospun and solution blown threedimensional carbon fiber nonwovens for application as electrodes in microbial fuel cells. Ener Environ Sci 4:1417-1421.
- 138. Sotiropoulou S, Chaniotakis NA (2003) Carbon nanotube array-based biosensor. Anal Bioanal Chem 375: 103-105.
- Sotiropoulou S, Gavalas V, Vamvakaki V, Chaniotakis NA (2003) Novel carbon materials in biosensor systems. Biosens Bioelectron 18: 211-215.
- 140.Bessel CA, Laubernds K, Rodriguez NM, Baker RTK (2001) Graphite nanofibers as an electrode for fuel cell applications. J Phys Chem B 105:1115– 1118.
- 141. Armstrong FA, Hill HAO, Walton NJ (1988) Direct electrochemistry of redox proteins. Acc Chem Res 21:407–413.
- 142. Frew JE, Hill HA (1988) Direct and indirect electron transfer between electrodes and redox proteins. Eur J Biochem 172: 261-269.
- 143. Taniguchi I, Yoshimoto S, Nishiyama K (1997) Effect of the structure of modifiers adsorbed on gold single crystal surfaces on the promotion of the electrode reaction of cytochrome c. Chem Lett 4:353–354.
- 144.Lamp BD, Hobara D, Porter MD, Niki K, Cotton TM (1997) Correlation of the structural decomposition and performance of pyridinethiolate surface modifiers at gold electrodes for the facilitation of cytochrome c heterogeneous electron-transfer reactions. Langmuir 13:736–741.
- 145. Hill HAO, Page DJ, Walton NJ (1987) Surface substitution-reactions at modified gold electrodes and their effect on the electrochemistry of horse heart cytochrome c. J Electroanal Chem 217: 141–158.
- 146.Xie Y, Dong S (1992) Effect of pH on the electron transfer of cytochrome c on a gold electrode modified with bis(4-pyridyl)disulphide. Bioelectrochem Bioenerg 29:71–79.
- 147. Allen PM, Allen H, Hill O, Walton NJ (1984) Surface modifiers for the promotion of direct electrochemistry of cytochrome c. J Electroanal Chem 178:69–86.
- 148. Feng YF, Yang XY, Di Y, Du YC, Zhang YL, et al. (2006) Mesoporous silica materials with an extremely high content of organic sulfonic groups and their comparable activities with that of concentrated sulfuric acid in catalytic esterification. J Phys Chem B 110: 14142-14147.
- 149. Bhatia RB, Brinker CJ, Gupta AK, Singh AK (2000) Aqueous sol-gel process for protein encapsulation. Chem Mat 12:2434–2441
- 150. Liu B, Hu R, Deng J (1997) Fabrication of an amperometric biosensor based on the immobilization of glucose oxidase in a modified molecular sieve matrix. Anal 122:821–826.
- 151.Liu B, Cao Y, Chen D, Kong J, Deng J (2003) Amperometric biosensor based on a nanoporous ZrO, matrix. Anal Chim Acta 478:59–66.
- 152. Heilmann A, Teuscher N, Kiesow A, Janasek D, Spohn U (2003) Nanoporous aluminum oxide as a novel support material for enzyme biosensors. J Nanosci Nanotechnol 3: 375-379.
- 153. Benetton XD, Navarro-Avila SG, Carrera-Figueiras C (2010) Electrochemical evaluation of ti/tio2-polyaniline anodes for microbial fuel cells using hypersaline microbial consortia for synthetic-wastewater treatment. J New Mat Electrochem Sys 13, 1-6.
- 154.Pant D, Van Bogaert G, De Smet M, Diels L, Vanbroekhoven K (2010) Use of novel permeable membrane and air cathodes in acetate microbial fuel cells. Electrochim Acta 55:7710–7716.
- 155. Alvarez-Gallego Y, Dominguez-Benetton X, Pant D, Diels L, Vanbroekhoven K, Genné I, Vermeiren P (2012) Development of gas diffusion electrodes for cogeneration of chemicals and electricity. Electrochim Acta 82:415–426.
- 156.Wang Z-G, Wan L-S, Liu Z-M, Huang X-J, Xu Z-K (2009) Enzyme immobilization on electrospun polymer nanofibers: An overview. J Mol Cat B Enz 56:189–195.

- 157. Sarma AK, Vatsyayan P, Goswami P, Minteer SD (2009) Recent advances in material science for developing enzyme electrodes. Biosens Bioelectron 24: 2313-2322.
- 158.Zheng L, Yao X, Li J (2006) Layer-by-layer assembly films and their applications in electroanalytical chemistry. Curr Anal Chem 2:279–296.
- 159. Fuentes M, Maquiese JV, Pessela BCC, Abian O, Fernandez-Lafuente R, Mateo C, Guisan JM (2004) New cationic exchanger support for reversible immobilization of proteins. Biotechnol Prog 20: 284-288.
- 160. Haccoun J, Piro B, Noël V, Pham MC (2006) The development of a reagentless lactate biosensor based on a novel conducting polymer. Bioelectrochemistry 68: 218-226.
- 161.Linford R, Schlindwein W (2006) Medical applications of solid state ionics. Sol State Ion 177:1559–1565.
- 162. Updike SJ, Hicks GP (1967) The enzyme electrode. Nature 214: 986-988.
- 163. Chen T, Barton SC, Binyamin G, Gao Z, Zhang Y, et al. (2001) A miniature biofuel cell. J Am Chem Soc 123: 8630-8631.
- 164.Barrière F, Kavanagh P, Leech D (2006) A laccase–glucose oxidase biofuel cell prototype operating in a physiological buffer. Electrochim Acta 51:5187– 5192.
- 165. Tsujimura S, Kano K, Ikeda T (2002) Glucose/O₂ biofuel cell operating at physiological conditions. Electrochem 70: 940–942.
- 166.Ammam M, Fransaer J (2010) Micro-biofuel cell powered by glucose/ O2 based on electro-deposition of enzyme, conducting polymer and redox mediators: preparation, characterization and performance in human serum. Biosens Bioelectron 25: 1474-1480.
- 167. Mano N, Mao F, Heller A (2003) Characteristics of a miniature compartmentless glucose-O2 biofuel cell and its operation in a living plant. J Am Chem Soc 125: 6588-6594.
- 168. Klibanov AM (1983) Immobilized enzymes and cells as practical catalysts. Science 219: 722-727.
- 169. Nagel B, Warsinke A, Katterle M (2007) Enzyme activity control by responsive redoxpolymers. Langmuir 23: 6807-6811.
- 170.Zussman E (2011) Encapsulation of cells within electrospun fibers. Polymer Adv Technol 22:366–371.
- 171.Katz E, Yarin AL, Salalha W, Zussman E (2006) Alignment and self-assembly of elongated micronsize rods in several flow fields. J Appl Phys 100:034313.
- 172. Bellan LM, Cross JD, Strychalski EA, Moran-Mirabal J, Craighead HG (2006) Individually resolved DNA molecules stretched and embedded in electrospun polymer nanofibers. Nano Lett 6: 2526-2530.
- 173.Dersch R, Steinhart M, Boudriot U, Greiner A, Wendorff JH (2005) Nanoprocessing of polymers: applications in medicine, sensors, catalysis, photonics. Polymer Adv Technol 16:276–282.
- 174.Katz E, Pita M (2009) Biofuel cells controlled by logically processed biochemical signals: towards physiologically regulated bioelectronic devices. Chemistry 15: 12554-12564.
- 175. Jochems P, Satyawali Y, Van Roy S, Doyen W, Diels L, et al. (2011) Characterization and optimization of Î²-galactosidase immobilization process on a mixed-matrix membrane. Enzyme Microb Technol 49: 580-588.
- 176. Srikanth S, Pavani T, Sarma PN, Venkata Mohan S (2011) Synergistic interaction of biocatalyst with bio-anode as a function of electrode materials. Int J Hydrogen Energy 36:2271–2280.
- 177. Panels JE, Lee J, Park KY, Kang SY, Marquez M, et al. (2008) Synthesis and characterization of magnetically active carbon nanofiber/iron oxide composites with hierarchical pore structures. Nanotechnology 19: 455612.
- 178. Kovalenko GA, Tomashevskaya LG, Chuenko T V., Rudina NA, Perminova L V., Reshetilov AN (2011) Synthesis of catalytic filamentous carbon on a nickel/graphite catalyst and a study of the resulting carbon-carbon composite materials in microbial fuel cells. Kinetic Catal 52:564–572.
- 179.Zhu Y, Peng T, Li J Chinese (2004) A glucose biosensor based on the enzyme electrode with carbon nanotube/platinum nanoparticle. J Anal Chem 32: 1299–1303.

^{180.} Kandimalla VB, Ju H (2006) Binding of acetylcholinesterase to multiwall carbon

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nanotube-cross-linked chitosan composite for flow-injection amperometric detection of an organophosphorous insecticide. Chemistry 12: 1074-1080.

- 181.Ye J-S, Wen Y, Zhang WD, Cui H, Xu G, Sheu F-S (2005) Electrochemical biosensing platforms using phthalocyanine-functionalized carbon nanotube electrode. Electroanal 17:89–96.
- 182. Manso J, Mena ML, Yáñez-Sedeño P, Pingarrón J (2007) Electrochemical biosensors based on colloidal gold–carbon nanotubes composite electrodes. J Electroanal Chem 603:1–7.
- 183.Kamitaka Y, Tsujimura S, Setoyama N, Kajino T, Kano K (2007) Fructose/ dioxygen biofuel cell based on direct electron transfer-type bioelectrocatalysis. Phys Chem Chem Phys 9: 1793-1801.
- 184. Tsujimura S, Kamitaka Y, Kano K (2007) Diffusion-controlled oxygen reduction on multi-copper oxidase-adsorbed carbon aerogel electrodes without mediator. Fuel Cells 7:463–469.
- 185. Dumitru A, Morozan A, Ghiurea M, Scott K, Vulpe S (2008) Biofilm growth from wastewater on MWNTs and carbon aerogels. Phys Stat Solidi (A) Appl Mat 205:1484-1487.
- 186. Novoselov KS, Geim AK, Morozov SV, Jiang D, Zhang Y, et al. (2004) Electric field effect in atomically thin carbon films. Science 306: 666-669.
- 187. Stoller MD, Park S, Zhu Y, An J, Ruoff RS (2008) Graphene-based ultracapacitors. Nano Lett 8: 3498-3502.
- Wang P (2006) Nanoscale biocatalyst systems. Curr Opin Biotechnol 17: 574-579.
- 189.Liu H, Gao J, Xue M, Zhu N, Zhang M, et al. (2009) Processing of graphene for electrochemical application: noncovalently functionalize graphene sheets with water-soluble electroactive methylene green. Langmuir 25: 12006-12010.
- 190. Kwon KY, Youn J, Kim JH, Park Y, Jeon C, et al. (2010) Nanoscale enzyme reactors in mesoporous carbon for improved performance and lifetime of biosensors and biofuel cells. Biosens Bioelectron 26: 655-660.
- 191.Kim MI, Kim J, Lee J, Jia H, Na HB, et al. (2007) Crosslinked enzyme aggregates in hierarchically-ordered mesoporous silica: a simple and effective method for enzyme stabilization. Biotechnol Bioeng 96: 210-218.
- 192. Piao Y, Lee D, Lee J, Hyeon T, Kim J, et al. (2009) Multiplexed immunoassay using the stabilized enzymes in mesoporous silica. Biosens Bioelectron 25: 906-912.
- 193. Zhou M, Guo J, Guo LP, Bai J (2008) Electrochemical sensing platform based on the highly ordered mesoporous carbon-fullerene system. Anal Chem 80: 4642-4650.
- 194.Zhou M, Deng L, Wen D, Shang L, Jin L, et al. (2009) Highly ordered mesoporous carbons-based glucose/O2 biofuel cell. Biosens Bioelectron 24: 2904-2908.
- 195. Joo SH, Choi SJ, Oh I, Kwak J, Liu Z, et al. (2001) Ordered nanoporous arrays of carbon supporting high dispersions of platinum nanoparticles. Nature 412: 169-172.
- 196. Chang H, Joo SH, Pak C (2007) Synthesis and characterization of mesoporous carbon for fuel cell applications. J Mat Chem 17:3078-3088.
- 197. Upadhyayula VK, Deng S, Mitchell MC, Smith GB (2009) Application of carbon nanotube technology for removal of contaminants in drinking water: a review. Sci Total Environ 408: 1-13.
- 198. Zhang Y, Sun J, Hou B, Hu Y (2011) Performance improvement of air-cathode single-chamber microbial fuel cell using a mesoporous carbon modified anode. J Pow Sour 196:7458–7464.
- 199.Chmiola J, Yushin G, Dash RK, Hoffman EN, Fischer JE, Barsoum MW, Gogotsi Y (2005) Double-layer capacitance of carbide derived carbons in sulfuric acid. Electrochem Solid-State Let 8:A357-A360
- 200. Daniel MC, Astruc D (2004) Gold nanoparticles: assembly, supramolecular chemistry, quantum-size-related properties, and applications toward biology, catalysis, and nanotechnology. Chem Rev 104: 293-346.
- 201.Deng Z, Dai Y, Chen W, Pei X, Liao J (2010) Synthesis and Characterization of Bowl-Like Single-Crystalline BaTiO(3) Nanoparticles. Nanoscale Res Lett 5: 1217-1221.
- 202. Templeton AC, Wuelfing WP, Murray RW (2000) Monolayer-protected cluster molecules. Acc Chem Res 33: 27-36.

- 203.Lu X, Zou G, Li J (2007) Hemoglobin entrapped within a layered spongy Co3O4 based nanocomposite featuring direct electron transfer and peroxidase activity. J Mat Chem 17:1427-1432.
- 204. Dyal A, Loos K, Noto M, Chang SW, Spagnoli C, et al. (2003) Activity of Candida rugosa lipase immobilized on gamma-Fe2O3 magnetic nanoparticles. J Am Chem Soc 125: 1684-1685.
- 205. Eggleston CM, Vörös J, Shi L, Lower BH, Droubay TC, Colberg PJS (2008) Binding and direct electrochemistry of OmcA, an outer-membrane cytochrome from an iron reducing bacterium, with oxide electrodes: A candidate biofuel cell system. Inorg Chim Acta 361:769–777.
- 206. Ansari SA, Husain Q (2012) Potential applications of enzymes immobilized on/ in nano materials: A review. Biotechnol Adv 30: 512-523.
- 207. Prakasam HE, Shankar K, Paulose M, Varghese OK, Grimes CA (2007) A new benchmark for TiO₂ nanotube array growth by anodization. J Phys Chem C 111:7235–7241.
- 208.Xie Y, Zhou L, Huang H (2007) Bioelectrocatalytic application of titania nanotube array for molecule detection. Biosens Bioelectron 22: 2812-2818.
- 209.Wu F, Xu J, Tian Y, Hu Z, Wang L, et al. (2008) Direct electrochemistry of horseradish peroxidase on TiO(2) nanotube arrays via seeded-growth synthesis. Biosens Bioelectron 24: 198-203.
- 210.Wu J, Suls J, Sansen W (1999) Amperometric glucose sensor with enzyme covalently immobilized by sol-gel technology. Anal Sci 15:1029–1032.
- 211. Wang J (1999) Sol–gel materials for electrochemical biosensors. Anal Chim Acta 399:21–27.
- 212. Nassif N, Livage J (2011) From diatoms to silica-based biohybrids. Chem Soc Rev 40: 849-859.
- 213. DiCarlo CM, Compton DL, Evans KO, Laszlo JA (2006) Bioelectrocatalysis in ionic liquids. Examining specific cation and anion effects on electrodeimmobilized cytochrome c. Bioelectrochemistry 68: 134-143.
- 214.Opallo M, Lesniewski A (2011) A review on electrodes modified with ionic liquids. J Electroanal Chem 656:2–16.
- 215. Silvester D.S., Rogers E.I., Compton R.G., McKenzie K.J., Ryder K.S., Endres F., McFarlane D., Abbott A.P. (2008) Electrodeposition from ionic liquids. Chapter 11. Technical aspects. Ed. Wiley VCH, Endres F., Abbott A.P. and MacFarlane D.R. Eds. 397 pp.
- 216. Wang M, Deng C, Nie Z, Xu X, Yao S (2009) The direct electrochemistry of glucose oxidase based on the synergic effect of amino acid ionic liquid and carbon nanotubes. Sci China Ser B: Chem 52:1991-1998.
- 217.Thomas G (Denver, CO, US), Ryne PR (Honeoye Falls, NY, US), Brian JL (Rochester, NY, US), Michael JH (Denver, CO, US) (2008) Carbon nanotube-polymer composite actuators. United States Department of Energy (Washington, DC, US) 7361430.
- 218.Si Y, Samulski ET (2008) Synthesis of water soluble graphene. Nano Lett 8: 1679-1682.
- 219. Yan Y, Zhang M, Gong K, Su L, Guo Z, Mao L (2005) Adsorption of methylene blue dye onto carbon nanotubes: a route to an electrochemically functional nanostructure and its layer-by-layer assembled nanocomposite. Chem Mat 17:3457–3463.
- 220.Lin Y, Zhu N, Yu P, Su L, Mao L (2009) Physiologically relevant online electrochemical method for continuous and simultaneous monitoring of striatum glucose and lactate following global cerebral ischemia/reperfusion. Anal Chem 81: 2067-2074.
- 221.Li X, Zhou H, Yu P, Su L, Ohsaka T, Mao L (2008) A Miniature glucose/ O2 biofuel cell with single-walled carbon nanotubes-modified carbon fiber microelectrodes as the substrate. Electrochem Comm 10:851–854.
- 222. Wang G, Xu JJ, Chen HY, Lu ZH (2003) Amperometric hydrogen peroxide biosensor with sol-gel/chitosan network-like film as immobilization matrix. Biosens Bioelectron 18: 335-343.
- 223. Chen Q, Long D, Chen L, Liu X, Liang X, Qiao W, Ling L (2011) Synthesis of ultrahigh-pore-volume carbon aerogels through a "reinforced-concrete" modified sol–gel process. J Non-Cryst Solid 357:232–235
- 224. Tian S, Liu J, Zhu T, Knoll W (2004) Polyaniline/gold nanoparticle multilayer films: assembly, properties, and biological applications. Chem Mat 16:4103– 4108.

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- 225. Willner I, Katz E, Patolsky F, Bückmann AF (1998) Biofuel cell based on glucose oxidase and microperoxidase-11 monolayer-functionalized electrodes. J Chem Soc, Perk Transact 2:1817–1822.
- 226.Pan C, Fang Y, Wu H, Ahmad M, Luo Z, et al. (2010) Generating electricity from biofluid with a nanowire-based biofuel cell for self-powered nanodevices. Adv Mater 22: 5388-5392.
- 227. Ivanov I, Vidakovic-Koch T, Sundmacher K (2010) Recent advances in enzymatic fuel cells: experiments and modeling. Energies 3:803–846.
- 228.Zebda A, Gondran C, Le Goff A, Holzinger M, Cinquin P, et al. (2011) Mediatorless high-power glucose biofuel cells based on compressed carbon nanotube-enzyme electrodes. Nat Commun 2: 370.
- 229. Coman V, Ludwig R, Harreither W, Haltrich D, Gorton L, et al (2009) A direct electron transfer-based glucose/oxygen biofuel cell operating in human serum. Fuel Cells 10:9.
- 230. Coman V, Vaz-Domínguez C, Ludwig R, Harreither W, Haltrich D, et al. (2008) A membrane-, mediator-, cofactor-less glucose/oxygen biofuel cell. Phys Chem Chem Phys 10: 6093-6096.
- 231. Wang X, Falk M, Ortiz R, Matsumura H, Bobacka J, et al. (2012) Mediatorless sugar/oxygen enzymatic fuel cells based on gold nanoparticle-modified electrodes. Biosens Bioelectron 31: 219-225.
- 232. Falk M, Andoralov V, Blum Z, Sotres J, Suyatin DB, et al. (2012) Biofuel cell as a power source for electronic contact lenses. Biosens Bioelectron 37: 38-45.
- 233.Larsson T, Elmgren M, Lindquist S-E, Tessema M, Gorton L, Henriksson G (1996) Electron transfer between cellobiose dehydrogenase and graphite electrodes. Anal Chim Acta 331:207–215.
- 234. Feng W, Ji P (2011) Enzymes immobilized on carbon nanotubes. Biotechnol Adv 29: 889-895.
- 235. Wu X, Zhao F, Varcoe JR, Thumser AE, Avignone-Rossa C, et al. (2009) A one-compartment fructose/air biological fuel cell based on direct electron transfer. Biosens Bioelectron 25: 326-331.
- 236. Sucheta A, Ackrell BA, Cochran B, Armstrong FA (1992) Diode-like behaviour of a mitochondrial electron-transport enzyme. Nature 356: 361-362.
- 237. Ramanavicius A, Kausaite A, Ramanaviciene A (2005) Biofuel cell based on direct bioelectrocatalysis. Biosens Bioelectron 20: 1962-1967.
- 238. Yaropolov AI, Karyakin AA, Varfolomeev SD, Berezin IV (1984) Mechanism of H₂-electrooxidation with immobilized hydrogenase. Bioelectrochem Bioenerg 12: 267-277
- 239. Vincent KA, Cracknell JA, Lenz O, Zebger I, Friedrich B, et al. (2005) Electrocatalytic hydrogen oxidation by an enzyme at high carbon monoxide or oxygen levels. Proc Natl Acad Sci U S A 102: 16951-16954.
- 240. Duine JA, Frank J, Verwiel PE (1980) Structure and activity of the prosthetic group of methanol dehydrogenase. Eur J Biochem 108: 187-192.
- 241. Ameyama M, Matsushita K, Ohno Y, Shinagawa E, Adachi O (1981) Existence of a novel prosthetic group, PQQ, in membrane-bound, electron transport chain-linked, primary dehydrogenases of oxidative bacteria. FEBS Lett 130: 179-183.
- 242. Jenkins P, Tuurala S, Vaari A, Valkiainen M, Smolander M, et al. (2012) A comparison of glucose oxidase and aldose dehydrogenase as mediated anodes in printed glucose/oxygen enzymatic fuel cells using ABTS/laccase cathodes. Bioelectrochemistry 87: 172-177.
- 243.Ohara TJ, Rajagopalan R, Heller A (1993) Glucose electrodes based on cross-linked [Os(bpy)2Cl]+/2+ complexed poly(1-vinylimidazole) films. Anal Chem 65: 3512-3517.
- 244. Vaze A, Hussain N, Tang C, Leech D, Rusling J (2009) Biocatalytic anode for glucose oxidation utilizing carbon nanotubes for direct electron transfer with glucose oxidase. Electrochem commun 11: 2004-2007.
- 245. Ivnitski D, Branch B, Atanassov P, Apblett C (2006) Glucose oxidase anode for biofuel cell based on direct electron transfer. Electrochem Comm 8:1204– 1210.
- 246.Guo CX, Li CM (2010) Direct electron transfer of glucose oxidase and biosensing of glucose on hollow sphere-nanostructured conducting polymer/ metal oxide composite. Phys Chem Chem Phys 12: 12153-12159.
- 247. Zayats M, Willner B, Willner I (2008) Design of amperometric biosensors and

biofuel cells by the reconstitution of electrically contacted enzyme electrodes. Electroanal 20:583–601.

- Bunte C, Prucker O, König T, Rühe J (2010) Enzyme containing redox polymer networks for biosensors or biofuel cells: a photochemical approach. Langmuir 26: 6019-6027.
- 249. Tamaki T, Hiraide A, Asmat FB, Ohashi H, Ito T, Yamaguchi T (2010) Evaluation of immobilized enzyme in a high-surface-area biofuel cell electrode made of redox-polymer-grafted carbon black. Ind Eng Chem Res 49:6394– 6398.
- 250.Heller A, Feldman B (2008) Electrochemical glucose sensors and their applications in diabetes management. Chem Rev 108: 2482-2505.
- 251.Heller A, Feldman B (2010) Electrochemistry in diabetes management. Acc Chem Res 43: 963-973.
- 252. Mano N, Mao F, Heller A (2005) On the parameters affecting the characteristics of the "wired" glucose oxidase anode. J Electroanal Chem 574:347–357.
- 253. Rajagopalan R, Aoki A, Heller A (1996) Effect of quaternization of the glucose oxidase "wiring" redox polymer on the maximum current densities of glucose electrodes. J Phys Chem 100: 3719-3727.
- 254.de Lumley-Woodyear T, Rocca P, Lindsay J, Dror Y, Freeman A, et al. (1995) Polyacrylamide-based redox polymer for connecting redox centers of enzymes to electrodes. Anal Chem 67: 1332-1338.
- 255. Gregg BA, Heller A (1991) Redox polymer films containing enzymes 2. Glucose oxidase containing enzyme electrodes. J Phys Chem B 95:5976–5980.
- 256. Rengaraj S, Mani V, Kavanagh P, Rusling J, Leech D (2011) A membraneless enzymatic fuel cell with layer-by-layer assembly of redox polymer and enzyme over graphite electrodes. Chem Commun (Camb) 47: 11861-11863.
- 257.Barrière F, Ferry Y, Rochefort D, Leech D (2004) Targeting redox polymers as mediators for laccase oxygen reduction in a membrane-less biofuel cell. Electrochem Comm 6:237–241.
- 258.Zhu Z, Momeu C, Zakhartsev M, Schwaneberg U (2006) Making glucose oxidase fit for biofuel cell applications by directed protein evolution. Biosens Bioelectron 21: 2046-2051.
- 259. Holland JT, Lau C, Brozik S, Atanassov P, Banta S (2011) Engineering of glucose oxidase for direct electron transfer via site-specific gold nanoparticle conjugation. J Am Chem Soc 133: 19262-19265.
- 260. Güven G, Prodanovic R, Schwaneberg U (2010) Protein engineering An option for enzymatic biofuel cell design. Electroanal 22:765–775.
- 261. Solomon EI, Sundaram UM, Machonkin TE (1996) Multicopper Oxidases and Oxygenases. Chem Rev 96: 2563-2606.
- 262. Santos SR, Maia G (2012) Direct charge transfer to horseradish peroxidase revisited using a glassy carbon electrode. Electrochim Acta 71:116-122.
- 263. Tarasevich MR, Bogdanovskaya VA, Zagudaeva NM, Kapustin AV (2002) Composite materials for direct bioelectrocatalysis of the hydrogen and oxygen reactions in biofuel cells. Russ J Electrochem 38: 335-335.
- 264. Tatsuma T, Watanabe T (1991) Peroxidase model electrodes: heme peptide modified electrodes as reagentless sensors for hydrogen peroxide. Anal Chem 63: 1580-1585.
- 265. Addo PK, Arechederra RL, Waheed A, Shoemaker JD, Sly WS, Minteer SD (2009) Methanol production via bioelectrocatalytic reduction of carbon dioxide: role of carbonic anhydrase in improving electrode performance. Electrochem Solid-State Lett 14:E9–E13.
- 266. Soukharev V, Mano N, Heller A (2004) A four-electron O(2)-electroreduction biocatalyst superior to platinum and a biofuel cell operating at 0.88 V. J Am Chem Soc 126: 8368-8369.
- 267.Palmore GTR, Kim H-H (1999) Electro-enzymatic reduction of dioxygen to water in the cathode compartment of a biofuel cell. J Am Chem Soc 464:110– 117.
- Solomon EI, Hadt RG (2011) Recent advances in understanding blue copper proteins. Coord Chem Rev 255:774–789.
- 269. Augustine AJ, Kjaergaard C, Qayyum M, Ziegler L, Kosman DJ, et al. (2010) Systematic perturbation of the trinuclear copper cluster in the multicopper oxidases: the role of active site asymmetry in its reduction of O2 to H2O. J Am Chem Soc 132: 6057-6067.

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- 270.Dos Santos L, Climent V, Blanford CF, Armstrong FA (2010) Mechanistic studies of the 'blue' Cu enzyme, bilirubin oxidase, as a highly efficient electrocatalyst for the oxygen reduction reaction. Phys Chem Chem Phys 12: 13962-13974.
- 271.Xu F (2001) Dioxygen reactivity of laccase: dependence on laccase source, pH, and anion inhibition. Appl Biochem Biotechnol 95: 125-133.
- 272.Beneyton T, Beyl Y, Guschin DA, Griffiths AD, Taly V, Schuhmann W (2011) The Thermophilic CotA Laccase from Bacillus subtilis: Bioelectrocatalytic Evaluation of O2 Reduction in the Direct and Mediated Electron Transfer Regime. Electroanal 23:1781–1789
- 273. Martins LO, Soares CM, Pereira MM, Teixeira M, Costa T, et al (2002) Molecular and biochemical characterization of a highly stable bacterial laccase that occurs as a structural component of the Bacillus subtilis endospore coat. J Biol Chem 277:18849–18859.
- 274. Yaropolov AI, Kharybin AN, Emnéus J, Marko-Varga G, Gorton L (1995) Flow-injection analysis of phenols at a graphite electrode modified with coimmobilised laccase and tyrosinase. Anal Chim Acta 308:137–144.
- 275. Weigel MC, Tritscher E, Lisdat F (2007) Direct electrochemical conversion of bilirubin oxidase at carbon nanotube-modified glassy carbon electrodes. Electrochem Comm 9:689–693.
- 276. Schubert K, Goebel G, Lisdat F (2009) Bilirubin oxidase bound to multi-walled carbon nanotube-modified gold. Electrochim Acta 54: 3033-3038.
- 277. Jönsson-Niedziolka M, Kaminska A, Opallo M (2010) Pyrene-functionalised single-walled carbon nanotubes for mediatorless dioxygen bioelectrocatalysis. Electrochim Acta 55:8744–8750.
- 278. Szot K, Nogala W, Niedziolka-Jönsson J, Jönsson-Niedziolka M, Marken F, Rogalski J, et al (2009) Hydrophilic carbon nanoparticle-laccase thin film electrode for mediatorless dioxygen reduction. Electrochim Acta 54:4620–4625.
- 279. Nogala W, Celebanska A, Szot K, Wittstock G, Opallo M (2010) Bioelectrocatalytic mediatorless dioxygen reduction at carbon ceramic electrodes modified with bilirubin oxidase. Electrochim Acta 55:5719–5724.
- 280.Zloczewska A, Jönsson-Niedziolka M, Rogalski J, Opallo M (2011) Vertically aligned carbon nanotube film electrodes for bioelectrocatalytic dioxygen reduction. Electrochim Acta 56:3947–3953.
- Dagys M, Haberska K, Shleev S, Arnebrant T, Kulys J, et al (2011) Laccasegold nanoparticle assisted bioelectrocatalytic reduction of oxygen. Electrochem Comm 12: 933-935.
- 282. Tsujimura S, Kano K, Ikeda T (2005) Bilirubin oxidase in multiple layers catalyzes four-electron reduction of dioxygen to water without redox mediators. J Electroanal Chem 576:113–120.
- 283.Blanford CF, Heath RS, Armstrong FA (2007) A stable electrode for highpotential, electrocatalytic O(2) reduction based on rational attachment of a blue copper oxidase to a graphite surface. Chem Commun (Camb) : 1710-1712.
- 284. Trudeau F, Daigle F, Leech D (1997) Reagentless mediated laccase electrode for the detection of enzyme modulators. Anal Chem 69: 882-886.
- 285. Wikström M, Verkhovsky MI (2006) Towards the mechanism of proton pumping by the haem-copper oxidases. Biochim Biophys Acta 1757: 1047-1051.
- 286. Colmati F, Yoshioka SA, Silva VLVB, Varela H, Gonzalez ER (2007) Enzymatic based biocathode in a polymer electrolyte membrane fuel cell. Int J Electrochem Sci 2: 195-202.
- 287. Pizzariello A, Stred'ansky M, Miertus S (2002) A glucose/hydrogen peroxide biofuel cell that uses oxidase and peroxidase as catalysts by composite bulkmodified bioelectrodes based on a solid binding matrix. Bioelectrochemistry 56: 99-105.
- 288. Aburto J, Ayala M, Bustos-Jaimes I, Montiel C, Terrés E, Domínguez JM, Torres E (2005) Stability and catalytic properties of chloroperoxidase immobilized on SBA-16 mesoporous materials. Micro Meso Mat 83:193–200.
- 289.Zhao W, Wu XQ, Lu ZQ, Hou WJ, Li HX (2010) Electrochemical studies of chloroperoxidase on poly-L-lysine film modified GC electrode. Chinese Chem Lett 21:93–96.
- 290. Palmore GT, Bertschy H, Bergens SH, Whitesides GM (1998) A methanol/ dioxygen biofuel cell that uses NAD-dependent dehydrogenases as catalysts: application of an electro-enzymatic method to regenerate nicotinamide adenine dinucleotide at low overpotentials. J Electroanal Chem 443: 155-161.

- 291. Akers NL, Moore CM, Minteer SD (2005) Development of alcohol/O2 biofuel cells using salt-extracted tetrabutylammonium bromide/Nafion membranes to immobilize dehydrogenase enzymes. Electrochim Acta 50: 2521-2525.
- 292. Thomas TJ, Ponnusamy KE, Chang NM, Galmore K, Minteer SD (2003) Effects of annealing on mixture-cast membranes of Nafion and quaternary ammonium bromide salts. J Mem Sci 213: 55-66.
- 293.Zhu Z, Sun F, Zhang X, Zhang Y-HP (2012) Deep oxidation of glucose in enzymatic fuel cells through a synthetic enzymatic pathway containing a cascade of two thermostable dehydrogenases. Biosens Bioelectron 36:110–5
- 294.Kim YH, Campbell E, Yu J, Minteer SD, Banta S (2013) Complete oxidation of methanol in biobattery devices using a hydrogel created from three modified dehydrogenases. Angew Chem Int Ed Engl 52: 1437-1440.
- 295. Sokic-Lazic D, Minteer SD (2008) Citric acid cycle biomimic on a carbon electrode. Biosens Bioelectron 24: 945-950.
- 296. Moehlenbrock MJ, Toby TK, Waheed A, Minteer SD (2010) Metabolon catalyzed pyruvate/air biofuel cell. J Am Chem Soc 132: 6288-6289.
- 297. Moehlenbrock MJ, Toby TK, Pelster LN, Minteer SD (2011) Metabolon catalysts: An efficient model for multi-enzyme cascades at electrode surfaces. Chemcatchem 3: 561-570.
- 298. Sokic-Lazic D, Minteer SD (2009) Pyruvate/air enzymatic biofuel cell capable of complete cxidation. Electrochem Solid-State Lett 12:F26-F28.
- 299. Arechederra RL, Treu BL, Minteer SD (2007) Development of glycerol/O2 biofuel cell. J Pow Sour 173: 156-161.
- 300. Arechederra RL, Minteer SD (2009) Complete oxidation of glycerol in an enzymatic biofuel cell. Fuel Cells 9: 63-69.
- 301.Arechederra MN, Jenkins C, Rinc RA, Artyushkova K, Atanassov P, et al (2010) Chemical polymerization and electrochemical characterization of thiazines for NADH electrocatalysis applications. Electrochim Acta 55: 6659-6664.
- 302. Tasca F, Gorton L, Kujawa M, Patel I, Harreither W, et al. (2010) Increasing the coulombic efficiency of glucose biofuel cell anodes by combination of redox enzymes. Biosens Bioelectron 25: 1710-1716.
- 303.Pant D, Van Bogaert G, Diels L, Vanbroekhoven K (2012) A comparative assessment of bioelectrochemical systems (BESs) and enzymatic fuel cells (EFCs): Microbial Biotechnology – Energy and Environment. Rajesh Arora (Ed) CAB International. Oxon, UK: 39-57.
- 304.Pant D, Singh A, Van Bogaert G, Irving Olsen S, Singh Nigam P, Diels L, Vanbroekhoven K (2012) Bioelectrochemical systems (BES) for sustainable energy production and product recovery from organic wastes and industrial wastewaters. RSC Adv 2(4):1248
- 305. Park DH, Zeikus JG (1999) Utilization of electrically reduced neutral red by Actinobacillus succinogenes: physiological function of neutral red in membrane-driven fumarate reduction and energy conservation. J Bacteriol 181: 2403-2410.
- 306. Nevin KP, Woodard TL, Franks AE, Summers ZM, Lovley DR (2010) Microbial electrosynthesis: feeding microbes electricity to convert carbon dioxide and water to multicarbon extracellular organic compounds. MBio 1.
- 307.Cheng S, Xing D, Call DF, Logan BE (2009) Direct biological conversion of electrical current into methane by electromethanogenesis. Environ Sci Technol 43: 3953-3958.
- 308. Villano M, Aulenta F, Ciucci C, Ferri T, Giuliano A, Majone M (2010) Bioelectrochemical reduction of CO(2) to CH(4) via direct and indirect extracellular electron transfer by a hydrogenophilic methanogenic culture. Bioresource technology 101: 3085–90.
- 309. Srikanth S, Reddy MV, Mohan SV (2012) Microaerophilic microenvironment at biocathode enhances electrogenesis with simultaneous synthesis of polyhydroxyalkanoates (PHA) in bioelectrochemical system (BES). Bioresour Technol 125: 291-299.
- Guterl J-K, Sieber V (2013) Biosynthesis "debugged": Novel bioproduction strategies. Engineering in Life Sciences 13: 4–18.
- 311. Jensen JU, Bandur V, Bjerrum NJ, Jensen SH, Ebbesen S, Mogensen M, Tophoj N, Yde L (2008) Pre-Investigation of water electrolysis. Report PSO-F&U 2006-1-6287. Technical University of Denmark and DONG Energy. Danish Public Service Obligation programme (PSO).

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- 312. Davenport RJ, Schubert FH (1991) Space water electrolysis: space station through advanced missions. J Pow Sour 36: 235–250.
- 314.Sevda S, Dominguez-Benetton X, Vanbroekhoven K, De Wever H, Sreekrishnan TR, Pant D (2013) High strength wastewater treatment accompanied by power generation using air cathode microbial fuel cell. Applied Energy 105: 194–206.
- Bullen RA, Arnot TC, Lakeman JB, Walsh FC (2006) Biofuel cells and their development. Biosens Bioelectron 21: 2015-2045.

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