

Bioengineering for Stem Cell-Based Cardiac Regeneration

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Cardiovascular disease remains the leading cause of death worldwide. A boundary for conventional severe heart failure treatments exists in spite of significant advances in therapeutic modalities and risk-reduction strategies [1]. This health problem has prompted research into new therapeutic approaches including cardiac regeneration [2]. With the discovery of various stem cell populations possessing cardiogenic potential, and the subsequent ability to isolate and expand these cells, the notion of a stem cell-based regenerative therapy has begun to take shape [3].

Acute ischemic injury and chronic cardiomyopathies lead to permanent loss of cardiac tissue leading to heart failure and a high rate of morbidity and mortality. For these pathologic conditions, cell transplantation is thought to be an emerging therapeutic method for replacing lost myocardium, and stem cell research and clinical trials for cardiac cell therapy are now being prioritized and funded in multiple countries [4,5]. Many clinical studies have been conducted using these somatic stem cells so far: TOPCAREAMI [6], BOOST [7], REPAIR-AMI [8] (Bone marrow hematopoietic stem cells), REGENT [9] (endothelial progenitor cells), POSEIDON [10] (mesenchymal stem cells), MAGIC [11], CAuSMIC [12] (skeletal myoblasts), CADUCEUS [13], SCIPIO5 (cardiac progenitor/stem cells) and so on. However, this field still lacks sufficiently conclusive results to support full-scale implementation of such therapies. A major reason for the insufficient results would be the poor survival and long-term engraftment of transplanted cells. Despite initial positive results on myocardial function and perfusion, the disappearance of transplanted cells reduces the likelihood of sustained positive paracrine effects or sustained recovery of function [14]. It is reported that more than 70% of the cells die during the first 48 hours after needle injection due to the hypoxic, inflammatory, and/or fibrotic environment [15]. Thus, new strategies such as combination of cardiac cells with bioengineering techniques are being subjected to intense research, suggesting that the strategies may improve the efficiency of stem cell therapies [16,17].

Initial experiments were performed by combining the cells with injectable biomaterials such as collagen, fibrin, gelatin, or Matrigel with the goal of providing a favorable microenvironment rich in growth factors. These early studies showed an increased survival of the grafted cells and an improvement of the cardiac function after transplantation [18-21]. However, these approaches did not accomplish the goal of sustained cell retention or an adequate distribution of the grafted cells. The creation of cellular patches as a tissue-like structure has been developed by using biomaterials which act as a delivery platform for the cells, assuring their engraftment and more homogeneous and organized distribution of the cells [17]. Cellular patches using mesenchymal stem cells (MSCs) entrapped in a collagen-I matrix and transplanted onto rat infarcted hearts induced an increase of cell engraftment and a functional improvement [22]. Three-dimensional (3D) contractile loops of mixed collagen and neonatal cardiomyocytes (CMs) have also been successfully used in rodent cardiac repair experiments. Implantation of these engineered heart tissues onto the damaged heart improved contractile function [23]. We have developed a novel 3D

engineered cardiac tissue (ECT) using chick or rat embryonic/fetal/ neonatal CMs and scaffolds as a robust in vitro model to investigate the maturing embryonic myocardium [24,25]. Recently, we found that mechanical stretch or p38 mitogen-activated protein kinase inhibition affects cellular development, growth or proliferation using gene expression assays with rat embryonic ECTs [26]. On the other hand, porous biomaterials, such as alginate or polymers like poly-glycolidecolactide, have also been tested as cell scaffolds with human embryonic stem (ES) cell-derived CMs [27]. New strategies like microtemplating or electrospinning have also been incorporated to create scaffolds that mimic the natural heart extracellular matrices to control a homogenous seeding of the cells allowing an organized and aligned distribution [28]. The repopulation of a decellularized mouse heart as extracellular matrices of the whole heart with human induced pluripotent stem cell (iPSC)-derived cardiovascular progenitor cells has also been reported [29].

Another promising approach for construction of 3D tissue-like structure is the creation of cell sheets or patches without scaffold support. The generation of cell sheets using monolayer cell culture is a promising method because of larger scalability and accessibility. This technique can be used with a culture dish covalently grafted with temperature-responsive polymer poly (N-isopropylacrylamide) (PIPAAm) which enables the preparation of cell sheets without enzymatic digestion [30]. The beneficial potential of this technique has been demonstrated by many experiments using stem cell sources such as the transplantation of a monolayer cell sheet generated from iPSCs or adipose tissue-derived MSCs to animal myocardial infarction models [31,32]. We have reported a transplantation study of a threelayered cardiac tissue sheet bioengineered with mouse embryonic stem cell (ESC)-derived defined cardiac cell populations to an infarcted rat heart [33]. In these cases, an increase in neovascularization together with an attenuation of ventricular remodeling responsible for the improvement in cardiac function has been demonstrated and this cell sheet-based method creates a novel platform for exploring the cellular mechanisms of cardiac regeneration. The combinations of cell types composing the transplanted cell sheets enabled us to elucidate the regenerative function of each cell type (for example, the comparison of cell sheets with or without CMs is helpful for the elucidation of

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the cellular function of CMs). This cell-type controlled analysis led us to identify one of the cellular mechanisms of cardiac regeneration following cell therapy that CMs are main contributors for the functional improvement through neovascularization.

Nevertheless the progresses in bioengineered technologies toward cardiac stem cell therapy introduced here, hurdles still remain for producing and adequate quantity of functional cardiac cells which do not die following implantation and for creating patches/organs that can mimic the structure and function of the heart. In this regard, iPSCs possess great potential for cardiac regeneration. A main reason is that iPSCs can be expanded geometrically in vitro while remaining pluripotent in an undifferentiated state in culture, and can give rise to most somatic cell lineages including various cardiac cells once allowed to differentiate [34]. In this regard, the regenerative capacity is theoretically limitless [35]. The merit of iPSCs is larger especially for the heart compared to other organs, such as endocrine or sensory organs, as the heart functions as an assembly of a large number of cells including CMs and other cell types (e.g. vascular cells, cardiac fibroblasts), and numerous heart-composing cells might be required to fully compensate for the damaged human heart [36]. Potent differentiation methods based on high-density monolayer culture and chemically defined factors, and modifications thereof, have been reported to induce CMs from human iPSCs with a robust efficiency of 40-70 % [37,38]. The application of these methods would strongly promote cardiac regeneration using human iPSCs. Another advantage of iPSCs is that they lack the ethical and immunogenic issues associated with the use of ESCs [4]. The generation of iPSCs by reprogramming autologous somatic cells with genes regulating pluripotency may resolve the ethical and immunogenic issues associated with the use of ESCs which is brought from inner cell mass with destruction of fertilized egg. Integration of bioengineering and iPSC technologies may generate an ideal structure suitable for cardiac regenerative therapy in the future.

The combination of cell therapy and local administration of cytokines that induce paracrine effects such as angiogenesis is a method for enhancing therapeutic potential of cell therapy. Tabata et al. [39] have developed a bioengineered system for sustained release of angiogenic cytokines, such as basic fibroblast growth factor (bFGF), from a biodegradable material, gelatin hydrogel; this system enables to control the release of cytokines over the periods required for efficient clinical outcomes. The addition of such sustained release of bFGF enhanced the functional benefit of the transplantation of cardiac progenitor cells in a porcine myocardial infarction (MI) model [40].

Besides cell-based strategy, there are promising approaches for cardiac regeneration with bioengineered technologies. Gene therapy is emerging as a potential treatment option in patients suffering from a wide spectrum of cardiovascular diseases [41]. Gene therapy, which is the direct introduction of transgenes into the vasculature or myocardium, may contribute in controlling the symptoms of cardiovascular diseases and may also reverse the pathological conditions involved. In 2010, Ieda et al. [42] reported that a combination of 3 developmental transcription factors (Gata4, Mef2c, and Tbx5) rapidly, efficiently, and directly reprogrammed postnatal cardiac or dermal fibroblasts into differentiated cardiomyocyte-like cells in vitro (direct reprogramming). This technology was recently applied to an in vivo mouse MI model in which the 3 genes were delivered by a retroviral vector, resulting in direct reprogramming of cardiac fibroblasts within the infarction site into cardiomyocyte-like cells and amelioration of cardiac dysfunction [43]. Three goals must be accomplished for appropriate gene therapy: suitable vectors must be generated, a suitable gene or group of genes must be identified, and an appropriate delivery system must be developed. Bioengineered materials such as biodegradable hydrogel are reported to contribute to this appropriate delivery of vectors and enhance the transfection efficiency with sustained release of vectors [44]. Thus, there a range of cellular and tissue engineering strategies are rapidly transitioning from pre-clinical to clinical trials to repair and regenerate damaged myocardium towards sustained recovery. We sincerely expect that these advanced modalities that integrate cellular and bioengineering technologies will enhance the efficacy of cardiac cell therapy and further contribute to cardiac regenerative medicine.

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